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012804

16138 U.S. PTO

PROVISIONAL APPLICATION FOR PATENT COVER SHEET

This is a request for filing a PROVISIONAL APPLICATION FOR PATENT under 37 CFR 1.53 (c).

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INVENTOR(S)					
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Stanton R.	Cantor	Tarzana, California USA			
<input type="checkbox"/> Additional Inventors are being named on the ___ separately numbered sheets attached hereto					
TITLE OF THE INVENTION (500 characters max)					
ANCHORING ELEMENT FOR USE IN BONE					
Direct all correspondence to: CORRESPONDENCE ADDRESS					
<input checked="" type="checkbox"/> Customer Number		<div style="border: 1px solid black; padding: 2px; display: inline-block;">08791</div>			
OR		Type Customer Number here			
<input type="checkbox"/> Firm or Individual Name	Blakely, Sokoloff, Taylor & Zafman LLP				
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City	Los Angeles	State	California	ZIP	90025
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ENCLOSED APPLICATION PARTS (check all that apply)					
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<input type="checkbox"/> Application Data Sheet. See 37 CFR 1.76					
METHOD OF PAYMENT OF FILING FEES FOR THIS PROVISIONAL APPLICATION FOR PATENT (check one)					
<input checked="" type="checkbox"/> Applicant claims small entity status. See 37 CFR 1.27.				<div style="border: 1px solid black; padding: 5px; display: inline-block;">\$80.00</div>	
<input checked="" type="checkbox"/> A check or money order is enclosed to cover the filing fees					
<input checked="" type="checkbox"/> The Commissioner is hereby authorized to charge filing fees or credit any overpayment to Deposit Account Number: <u>02-2666</u>					
<input type="checkbox"/> Payment by credit card. Form PTO-2038 is attached.					
The invention was made by an agency of the United States Government or under a contract with an agency of the United States Government.					
<input checked="" type="checkbox"/> No					
<input type="checkbox"/> Yes, the name of the U.S. Government agency and the Government contract number are:					

Respectfully submitted,
SIGNATURETYPED or PRINTED NAME James Henry

TELEPHONE

Date 1/28/2004REGISTRATION NO. 41,064
(if appropriate)Docket Number: 2184P002Z**USE ONLY FOR FILING A PROVISIONAL APPLICATION FOR PATENT**22151 U.S. PTO
60/539633

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FEE TRANSMITTAL for FY 2003

Effective 01/01/2003. Patent fees are subject to annual revision.

☒ Applicant claims small entity status. See 37 CFR 1.27.

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Application Number
Filing Date
First Named Inventor Stanton R. Cantor
Examiner Name
Group/Art Unit
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METHOD OF PAYMENT (check all that apply)

☒ Check ☐ Credit card ☐ Money Order ☐ Other ☐ None
☒ Deposit Account

Deposit Account Number 02-2666
Deposit Account Name Blakely, Sokoloff, Taylor & Zafman LLP

The Commissioner is authorized to: (check all that apply)

☒ Charge fee(s) indicated below ☐ Credit any overpayments
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FEE CALCULATION

1. BASIC FILING FEE

Large Entity		Small Entity		Fee Description	Fee Paid
Fee Code	Fee (\$)	Fee Code	Fee (\$)		
1001	770	2001	385	Utility filing fee	
1002	340	2002	170	Design filing fee	
1003	530	2003	265	Plant filing fee	
1004	770	2004	385	Reissue filing fee	
1005	160	2005	80	Provisional filing fee	80.00
SUBTOTAL (1)				(\$)	80.00

2. EXTRA CLAIM FEES

Total Claims - 20* = X =
Independent Claims - 3* = X =
Multiple Dependent =

Large Entity		Small Entity		Fee Description	Fee Paid
Fee Code	Fee (\$)	Fee Code	Fee (\$)		
1202	18	2202	9	Claims in excess of 20	
1201	86	2201	43	Independent claims in excess of 3	
1203	290	2203	145	Multiple Dependent claim, if not paid	
1204	86	2204	43	**Reissue independent claims over original patent	
1205	18	2205	9	**Reissue claims in excess of 20 and over original patent	
SUBTOTAL (2)				(\$)	

*or number previously paid, if greater, For Reissues, see below

FEE CALCULATION (continued)

3. ADDITIONAL FEES

Large Entity		Small Entity		Fee Description	Fee Paid
Fee Code	Fee (\$)	Fee Code	Fee (\$)		
1051	130	2051	65	Surcharge - late filing fee or oath	
1052	50	2052	25	Surcharge - late provisional filing fee or cover sheet.	
2053	130	2053	130	Non-English specification	
1812	2,520	1812	2,520	For filing a request for ex parte reexamination	
1804	920*	1804	920*	Requesting publication of SIR prior to Examiner action	
1805	1,840*	1805	1,840*	Requesting publication of SIR after Examiner action	
1251	110	2251	55	Extension for reply within first month	
1252	420	2252	210	Extension for reply within second month	
1253	950	2253	475	Extension for reply within third month	
1254	1,480	2254	740	Extension for reply within fourth month	
1255	1,210	2255	605	Extension for reply within fifth month	
1404	330	2401	165	Notice of Appeal	
1402	330	2402	165	Filing a brief in support of an appeal	
1403	290	2403	145	Request for oral hearing	
1451	1,510	2451	1,510	Petition to institute a public use proceeding	
1452	110	2452	55	Petition to revive - unavoidable	
1453	1,330	2453	665	Petition to revive - unintentional	
1501	1,330	2501	665	Utility issue fee (or reissue)	
1502	480	2502	240	Design issue fee	
1503	640	2503	320	Plant issue fee	
1460	130	2460	130	Petitions to the Commissioner	
1807	50	1807	50	Processing fee under 37 CFR 1.17(q)	
1806	180	1806	180	Submission of Information Disclosure Stmt	
8021	40	8021	40	Recording each patent assignment per property (times number of properties)	
1809	770	1809	385	Filing a submission after final rejection (37 CFR § 1.129(a))	
1810	770	2810	385	For each additional invention to be examined (37 CFR § 1.129(b))	
1801	770	2801	385	Request for Continued Examination (RCE)	
1802	900	1802	900	Request for expedited examination of a design application	

Other fee (specify) _____

* Reduced by Basic Filing Fee Paid

SUBTOTAL (3)

(\$)

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Date

01/28/04

Based on PTO/SB/17 (08-03) as modified by Blakely, Sokoloff, Taylor & Zafman (wlr) 08/11/2003.
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UNITED STATES PATENT APPLICATION
FOR
ANCHORING ELEMENT FOR USE IN BONE

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ANCHORING ELEMENT FOR USE IN BONE

BACKGROUND OF THE INVENTION

[0001] Anchoring elements are used in a variety of dental, medical, and surgical procedures where it is desired to embed a mechanical attachment into living bone. One example of a procedure that uses anchoring elements is dental prosthesis using embedded implants.

[0002] Dental implants provide a desirable prosthesis for patients who are missing one or more natural teeth. A dental implant includes an anchoring element that is embedded into the jawbone and a prosthetic tooth that is attached to and supported by the anchoring element. The prosthetic tooth may be attached directly to the anchoring element or an abutment fixture may be attached to the anchoring element and support the prosthetic tooth in turn. An appropriate anchoring element will support bone growth that invades the anchoring element such that the anchoring element becomes integrated with the surrounding bone in a process termed osseointegration.

[0003] An anchoring element to support a prosthetic tooth may be embedded in what is termed a two-stage procedure. In the first stage, the anchoring element is embedded into the jawbone and the surgical site is then closed. After a period of months the anchoring element will achieve osseointegration. The site of the anchoring element is then re-opened surgically to allow the attachment of a prosthetic tooth.

[0004] More recently techniques have been developed that permit a dental implant to be embedded in a one-stage procedure. In a one-stage procedure, the anchoring element is embedded and a prosthetic tooth is immediately fitted. The immediately fitted prosthetic tooth may be an interim prosthesis that allows the soft tissue to properly heal and maintains the spacing and alignment of adjacent teeth during the period of osseointegration. A permanent prosthetic tooth may be fitted at a later date after at least some osseointegration has occurred without requiring an additional surgical procedure.

[0005] To achieve successful osseointegration it is necessary that the anchoring element fit closely into the surrounding bone, generally having a

gap of no more than 1.5 millimeters. It is also important that the anchoring element not move relative to the surrounding bone during the period of osseointegration. Where the anchoring element cannot be closely fitted to the surrounding bone, it may be necessary to use bone-grafting materials to fill the space between the anchoring element and the surrounding bone.

[0006] Molars are commonly missing teeth. The use of an implant to replace a molar presents some special difficulties. Molars generally have multiple roots. The mandibular molars of the lower jaw generally have two roots. The maxillary molars of the upper jaw generally have three roots. In a fresh extraction site the void left by the molar roots presents a site that can be difficult to fit with an anchoring element. In addition, the bone in the molar region of the jaw generally consists of a thin hard layer of cortical bone surrounding a core of softer spongy cancellous bone. The cancellous bone may provide poor support for the anchoring element prior to osseointegration.

[0007] A molar is a relatively large tooth and it is desirable to use an anchoring element having a relatively large diameter to fill the void following an extraction. However, the use of a wide anchoring element may require that a significant amount of bone be removed from the extraction site to accommodate the anchoring element. This may leave only a small amount of cortical bone available to support the anchoring element which may be embedded in predominantly cancellous bone. In particular, the use of a wide anchoring element may require removal of the triangular mound-shaped mass of bone that is found between the roots known as the interradicular bone. Thus, it is difficult to place an anchoring element in a fresh molar extraction site with sufficient stability to allow embedding of a dental implant with a one-stage procedure.

[0008] Another circumstance that can present difficulties in placing an anchoring element for a dental implant occurs in cases where it is desired to place a dental prosthesis in a healed extraction site. When a molar is lost, the alveolar ridge that supports the teeth is fairly rapidly resorbed. This causes a loss of height of the jawbone in the area of tooth loss. When

an anchoring element is to be embedded in a healed extraction site, it may not be possible to place an anchoring element to a very great depth.

[0009] In the lower jaw, the presence of the mandibular alveolar nerve in the lower jaw limits the depth of the anchoring element. In the upper jaw the maxillary sinus limits the depth. These limiting anatomical features may require the use of a short anchoring element, perhaps 5 to 8 millimeters in length. The use of short anchoring elements for such cases has a lower rate of long-term success because of the reduced surface area available for osseointegration.

[0010] It would be desirable to have an anchoring element that can be used to place a dental implant in the molar area both for fresh extraction sites and for healed sites.

SUMMARY OF THE INVENTION

[0011] An anchoring element for use in bone has a proximal end and a distal end. The distal end may be embedded in bone with the proximal end exposed. An abutment surface is disposed toward the proximal end. The anchoring element includes four surfaces that define the distal end. A generally cylindrical first surface defines a exterior of the anchoring element. At least a portion of the first surface includes a first external thread having a pitch. An annular second surface is disposed toward the distal end and joined to the first concentric with the first surface is joined to the second surface along an inner surface along an outer circumference of the second surface. A third surface circumference of the second surface. At least a portion of the third surface includes an internal thread having the pitch of the first external thread. A fourth surface disposed between the distal end and the proximal end of the first surface is joined to the third surface along an outer circumference of the fourth surface.

[0012] In another embodiment, an anchoring element includes six surfaces that define the distal end. At least a portion of a first surface includes a first external thread. An annular second surface is disposed toward the distal end and joined to the first surface along an outer circumference of the second surface. A third surface concentric with the first surface is joined to the second surface along an inner circumference of the second surface. An annular fourth surface is disposed between the distal end and the proximal end and joined to the third surface along an outer circumference of the fourth surface. A fifth surface concentric with the first surface is joined to the fourth surface along an inner circumference of the fourth surface. A sixth surface is disposed toward the distal end and joined to the fifth surface along an outer circumference of the sixth surface.

[0013] In another embodiment, an anchoring element for use in bone has a proximal end and a distal end. The distal end may be embedded in bone with the proximal end exposed. The anchoring element includes a generally cylindrical first surface, at least a portion of the first surface including an external thread. An abutment surface is disposed at the

proximal end of the anchoring element. The abutment surface is at an angle to an axis from the proximal end to the distal end of the anchoring element.

BRIEF DESCRIPTION OF THE DRAWINGS

5 **[0014]** FIG. 1 is a pictorial view of an anchoring element for use in bone that embodies the invention.

[0015] FIG. 2 is a plan view of the distal end of the anchoring element shown in Figure 1.

10 **[0016]** FIG. 3 is a cross section of the anchoring element taken along the line 3—3 shown in Figure 2.

[0017] FIG. 4 is a plan view of the distal end of the anchoring element of Figures 1 through 3.

[0018] FIG. 5 is a side elevation of another anchoring element that embodies the invention.

15 **[0019]** FIG. 6 is a plan view of the proximal end of the anchoring element of Figure 5.

[0020] FIG. 7 is a cross section taken along section line 7—7 shown in Figure 6.

20 **[0021]** FIG. 8 is a plan view of the proximal end of the anchoring element of Figures 5 through 7.

[0022] FIG. 9 is a pictorial view of another anchoring element that embodies the invention.

[0023] FIG. 10 is a plan view of the proximal end of the anchoring element of Figure 9.

25 **[0024]** FIG. 11 is a cross section of the anchoring element taken along the line 11—11 shown in Figure 10.

[0025] FIG. 12 is a plan view of the distal end of the anchoring element of Figures 9 through 11.

30 **[0026]** FIG. 13 is a cross section of the anchoring element with the distal portion taken along the section line 13—13 shown in Figure 12 and the proximal portion taken along the section line 11—11 shown in Figure 10.

[0027] FIG. 14 is a cross section view of another anchoring element that embodies the invention.

[0028] FIG. 15 is a cross section of the anchoring element shown in Figure 14 with the distal portion sectioned similarly to the view of Figure 13.

5 [0029] FIG. 16 is a cross section of a mandibular molar extraction site.

[0030] FIG. 17 is a cross section of the extraction site shown in Figure 16.

[0031] FIG. 18 is a cross section similar to the view of Figure 16 showing the preparation of the extraction site for embedding an anchoring element.

[0032] FIG. 19 is a cross section of the upper portion of the extraction site
10 shown in Figure 18.

[0033] FIG. 20 is a cross section of the lower portion of the extraction site shown in Figure 18.

[0034] FIG. 21 is a cross section of an anchoring element embedded in the extraction site prepared as shown in Figure 18.

15 [0035] FIG. 22 is a cross section of a first part of another anchoring element that embodies the invention.

[0036] FIG. 23 is a side view of a second part of the anchoring element.

[0037] FIG. 24 is a view of the second part shown in side view installed into the first part shown in cross section to form the anchoring element.

20 [0038] FIG. 25 is a view of an alternate position for the second part relative to the first part of the anchoring element shown in Figure 24.

[0039] FIG. 26 is a cross section of a first part and side view of a second part forming another anchoring element that embodies the invention.

[0040] FIG. 27 is a cross section of a first part and side view of a second
25 part forming another anchoring element that embodies the invention.

[0041] FIG. 28 is a cross section of a first part of another anchoring element that embodies the invention.

[0042] FIG. 29 is a side view of a second part of the anchoring element.

[0043] FIG. 30 is a view of the second part shown in side view installed into
30 the first part shown in cross section to make the complete anchoring element.

[0044] FIG. 31 is a cross section of another anchoring element that embodies the invention.

[0045] FIG. 32 is a cross section of another anchoring element that embodies the invention.

[0046] FIG. 33 is a cross section of another anchoring element that embodies the invention shown as it may be embedded in bone.

5 **[0047]** FIG. 34 is a side view of another anchoring element that embodies the invention.

[0048] FIG. 35 is a side view of another anchoring element that embodies the invention.

DETAILED DESCRIPTION OF THE INVENTION

[0049] Figure 1 shows an anchoring element 100 for use in bone that embodies the invention. The anchoring element may be fabricated of any biocompatible material known or discovered to promote osseointegration such as titanium or a titanium alloy. The portions of that are to be in intimate contact with bone can display various surface characteristics. These portions can be titanium plasma sprayed, coated with hydroxy-apatite (HA coated), surface machined, sand blasted, or acid etched to promote osseointegration.

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10 **[0050]** For convenience in description, the anchoring element 100 will be described with reference to a distal end and a proximal end. The distal end is shown in Figure 1 as the end to the lower right and is the end that is embedded to the greatest depth in bone. The proximal end is the end to the upper right and is the end that may be exposed when the anchoring
15 element 100 is embedded in bone.

[0051] The anchoring element 100 includes a first surface that is a generally cylindrical exterior surface of the anchoring element. The term "generally cylindrical" is used to describe a surface that is substantially rotationally symmetric about an axis that extends from the distal end to the proximal
20 end. The first surface may include a screw thread 112. It will be appreciated that a screw thread is not rotationally symmetric in the strictest sense. A screw thread or similar feature is intended to be included by the term "substantially rotationally symmetric." The exterior surface of the anchoring element 100 may include features such as the aforementioned
25 screw thread and other features such as shoulders 102, tapered portions 110, and the like, all of which are intended to be included by the term "generally cylindrical."

[0052] At least a portion of the first surface of the anchoring element 100 may include a first external thread 112 having a pitch. The thread 112 may
30 be of any of a variety of forms known or discovered to be effective for embedding the anchoring element in bone. The thread 112 may include self-threading features or other features that aid in embedding the anchoring element into bone or that promote osseointegration.

- 5 **[0053]** The first surface may include a frustrated first conical portion 110 adjacent the distal end of the anchoring element 100 such that a smaller circumference of the first conical portion is adjacent the distal end. The first conical portion 110 may facilitate placing the anchoring element 100 into a hole that is prepared in the bone to receive the anchoring element. The first conical portion 110 may provide a somewhat smaller leading distal end that allows the anchoring element 100 to initially engage the bone with minimal force and align the anchoring element to the hole that has been prepared in the bone.
- 10 **[0054]** The first conical portion 110 may be unthreaded or may partially or fully intersect the first external thread 112. In one embodiment the first conical portion 110 may have a smallest diameter at the distal end of the anchoring element 100 that is approximately a root diameter of the first external thread. The first conical portion 110 may gradually increase in diameter toward the proximal end thereby providing a gradually increasing thread depth.
- 15 **[0055]** The anchoring element 100 may include an abutment surface disposed toward the proximal end of the first surface. The abutment surface may be of any of a variety of known or discovered forms that permit attachment to the anchoring element.
- 20 **[0056]** Figures 1 through 3 illustrate an abutment surface that may be provided to receive a dental prosthesis. The illustrated abutment surface includes an external hex surface 104 that may provide a wrenching surface for embedding the anchoring element 100. The illustrated abutment surface further includes a locating recess 106 and an internal anchoring thread 108 to receive a devices that is coupled to the anchoring element by a screw.
- 25 **[0057]** The anchoring element 100 includes an annular second surface 120 disposed toward the distal end of the first surface and joined to the first surface along an outer circumference 122 of the second surface. The second surface 120 may engage the bottom of the hole that has been prepared in the bone and thereby contribute significantly to the stability of the embedded anchoring element 100. The second surface 120 may be
- 30

substantially flat or may have a rounded or other shape chosen to effectively cooperate with the bottom of the hole that has been prepared in the bone to provide initial stability.

5 **[0058]** As may be seen in the plan view of the distal end, the anchoring element 100 includes a third surface 140 concentric with the first surface and joined to the second surface 120 along an inner circumference 124 of the second surface. At least a portion of the third surface 140 may include an internal thread having the pitch of the first external thread such that both threads will advance the anchoring element 100 at the same rate as it is
10 rotated to embed the anchoring element into bone. It is contemplated that the hole in the bone that is prepared to receive the anchoring element 100 may leave residual bone in place such that the third surface 140 will at least partially engage the bone to provide additional initial stability and an additional surface for osseointegration.

15 **[0059]** The third surface 140 may include a frustrated second conical portion adjacent the distal end such that a larger circumference of the second conical portion is adjacent the distal end. The second conical portion may facilitate placing the anchoring element 100 into the portion of hole that includes residual bone. The second conical portion may compress the
20 residual bone as the anchoring element 100 is embedded to further increase initial stability.

[0060] The second conical portion may be unthreaded or may partially or fully intersect the first internal thread 140. In one embodiment the second conical portion may have a largest diameter at the distal end of the
25 anchoring element 100 that is approximately a root diameter of the first internal thread. The second conical portion may gradually increase in diameter toward the proximal end thereby providing a gradually increasing thread depth.

[0061] The anchoring element 100 includes a fourth surface 130 disposed
30 between the distal end and the proximal end and joined to the third surface 140 along an outer circumference of the fourth surface 132. It is contemplated that the hole in the bone that is prepared to receive the anchoring element 100 may leave an upper surface on the residual bone

such that the fourth surface 130 will engage the upper surface to provide additional initial stability and an additional surface for osseointegration.

[0062] Figure 3 is a cross-section of the anchoring element 100 taken along a diameter as shown by the section line 3--3 in Figure 2. Figure 3 may aid in visualizing the relationships between the various surfaces of the anchoring element 100. Figure 3 may also aid in visualizing a possible interaction of the conical sections with the threads at the distal end.

[0063] Figures 5 through 8 illustrate another anchoring element 200 that embodies the invention. This embodiment includes many features that are similar to the anchoring element 100 illustrated by Figures 1 through 4. Similar features for anchoring element 200 have been given reference numerals that are the reference numerals used for anchoring element 100 increased by 100.

[0064] In this embodiment the anchoring element 200 includes an abutment surface 204 in the form of a frustrated square pyramid. The abutment surface 204 may provide a wrenching surface. If the anchoring element is used to support a dental prosthesis, a prosthetic tooth may be directly coupled to the abutment surface 204 such as by cement.

[0065] Figure 7 shows a cross section of the anchoring element 200 taken along the section line 7--7 as shown in the plan view of the proximal end of Figure 6. The first surface may be a slightly larger in diameter than the third surface. It may be seen in Figure 7 that there will be a comparatively thin cross-section where the roots of the external thread 212 coincide with the internal thread. It may be advantageous to arrange the internal threads so that the roots coincide with the crest of the external thread to avoid a thin cross section.

[0066] The anchoring element 200 may be relatively short such that if the first and/or third generally cylindrical surfaces include a conical section, the conical section may occupy all or substantially all of the first and/or third surfaces.

[0067] Figures 9 through 13 illustrate another anchoring element 300 that embodies the invention. This embodiment includes many features that are similar to the anchoring element 100 illustrated by Figures 1 through 4.

Similar features for anchoring element 300 have been given reference numerals that are the reference numerals used for anchoring element 100 increased by 200.

[0068] Figures 10 and 11 illustrate an abutment surface that may be provided to receive a dental prosthesis. The illustrated abutment surface includes a lobed locating recess 306 and an internal anchoring thread 308 to receive a device that is coupled to the anchoring element 300 by a screw. The lobes of the locating recess 306 may prevent rotation of a coupled device and may provide a wrenching surface for embedding the anchoring element 300.

[0069] In this embodiment the anchoring element the fourth surface 330 is annular. The anchoring element further includes a fifth surface 350 concentric with the first surface and joined to the fourth surface 330 along an inner circumference 334 of the fourth surface. A sixth surface 360 is disposed toward the distal end of the first surface and joined to the fifth surface 350 along an outer circumference 362 of the sixth surface.

[0070] The fifth surface 350 may include a second external thread on all or part of the fifth surface. The second external thread has the pitch of the first external thread such that all threads will advance the anchoring element 300 at the same rate as it is rotated to embed the anchoring element into bone. It is contemplated that the hole in the bone that is prepared to receive the anchoring element 300 may provide a secondary hole in the residual bone such that the fifth surface 350 will at least partially engage the bone to provide additional initial stability and an additional surface for osseointegration.

[0071] The fifth surface 350 may include a frustrated third conical portion adjacent the distal end such that a smaller circumference of the third conical portion is adjacent the distal end. The third conical portion may be unthreaded or may partially or fully intersect the second external thread on the fifth surface 350. In one embodiment the third conical portion may have a smallest diameter at the distal end of the anchoring element 300 that is approximately a root diameter of the second external thread. The third conical portion may gradually increase in diameter toward the proximal end

thereby providing a gradually increasing thread depth. The second and third conical sections may act to compress the residual bone between the third and fifth generally cylindrical surfaces.

5 [0072] Figure 13 is a cross-section view of anchoring element 300 shown in Figures 9-12 where the lower part of the cross-section is taken along section line 13--13 shown in Figure 12 so that the fifth surface is not cut by the cross-section and the fifth surface may be seen. The portion of the cross-section between the fourth surface 330 and the proximal end is taken along section line 11--11 shown in Figure 10.

10 [0073] Figures 14 and 15 illustrate another anchoring element 400 that embodies the invention. This embodiment includes many features that are similar to the anchoring element 300 illustrated by Figures 9 through 13. Similar features for anchoring element 400 have been given reference numerals that are the reference numerals used for anchoring element 300 increased by 100.

15 [0074] In this embodiment the anchoring element 400 the first surface includes a shoulder surface 402 in the form of a frustrated conical section. Such a conical shoulder is intended to be included by the term "generally cylindrical." The anchoring element 400 may be relatively short such that an internal anchoring thread 408 extends into the portion of the anchoring element 400 defined by the fifth surface 450.

[0075] Figures 16 through 20 illustrate an exemplary use of an anchoring element 500 that embodies the invention to provide a dental prosthesis for an extracted molar tooth.

25 [0076] Figure 16 shows a cross-section of a socket following the extraction of a mandibular molar having two roots. The cross-section is taken along a section line that is mesiodistal (running from the front to the back of the head). The socket includes the interradicular bone 510 which separated the roots of the extracted molar.

30 [0077] Figure 17 shows a cross-section of the socket viewed from the top and looking down into the socket. An outline of the cervical collar 512 taken along section line 17A--17A in Figure 16 is shown. An outline of

each of the two roots 514, 516 taken along section line 17B--17B in Figure 16 is shown.

5 [0078] Figure 18 shows a cross-section of the socket of Figure 16 after a hole has been prepared to receive the anchoring element. Figure 19 is a top down cross-section of the prepared hole at the cervical collar 512 taken along section line 19--19 in Figure 18. It may be seen the prepared hole 520 may not remove all of the cervical collar 512. Generally it is desirable to provide a large periphery of contact between the anchoring element 500 and the cervical collar 512 to provide good initial stability. However, it is also desirable to preserve as much bone as possible consistent with preparing a hole that will provide good initial stability and good osseointegration. In particular, the bone may have a relatively thin and hard cortical layer surrounding a softer inner core of cancellous bone. It is desirable preserve the cortical bone which will provide much more initial stability than the spongy cancellous bone.

15 [0079] The anchoring element 500 may be sized to come within at least 1.5 millimeters of all parts of the socket so that osseointegration will occur. The anchoring element 500 may be sized so that about 75% or more of the periphery at the cervical collar is in direct contact with the anchoring element to provide good initial stability.

20 [0080] Figure 20 shows a cross-section of the socket of Figure 16 after a hole has been prepared to receive the anchoring element. Figure 20 is a top down cross-section of the prepared hole at the roots 514, 516 taken along section line 20--20 in Figure 18. It may be seen the prepared hole 522 may not remove all of the socket that surrounded the roots. It may also be seen that a substantial portion of the interradicular bone 510 is preserved as residual bone in the prepared hole. The distal portion of the prepared hole 522 includes an annular region 524 to receive the portion of the anchoring implant between the first surface 501 and third surface 503. 25 If the anchoring element 500 includes a fifth surface 505, the prepared hole will include a secondary hole 526 in the residual interradicular bone.

30 [0081] The bottom surfaces 530, 532, 534 of the prepared hole are also significant. It is desirable that the bottom surfaces support a significant

portion of the second surface 502, fourth surface 504, and sixth surface 506 (if present) of the anchoring element 500. For this reason, the hole may be prepared with bottom surfaces 530, 534 that are below the lowest point of the roots if permitted by other anatomical structures such as the mandibular nerve 518 or maxillary sinus. A flat surface 532 may be prepared on the proximal portion of the residual interradicular bone 510 to support the fourth surface 504.

[0082] Figures 22 through 25 show another anchoring element 600 that embodies the invention. A first part 610 includes a first surface 601, a second surface 602, a third surface 603, and a fourth surface 604. A second part 620 includes a fifth surface 605 and a sixth surface 606. The fifth surface 605 is joined to the fourth surface 604 by screwing the second part 620 into the first part 610. The resulting assembly provides an anchoring element 600 that has similar features to the anchoring element 300 shown in Figure 9. It may be possible to adjust the position of the sixth surface 606 relative to the second surface 602 as shown by Figures 24 and 25.

[0083] Figure 26 shows another anchoring element 700 that embodies the invention. A second part 720 is screwed into a first part 710 to provide an anchoring element 700 that has similar features to the anchoring element 400 shown in Figure 14. The second part 720 may be shaped so that it can be screwed into an interference fit with the first part 710 such that the anchoring element 700 functions as a single piece after assembly.

[0084] Figure 27 shows another anchoring element 800 that embodies the invention. A second part 820 passes through an unthreaded opening 814 in a first part 810 to provide an anchoring element 800 that has similar features to the anchoring element 400 shown in Figure 14. The second part 820 may include a head surface 822 that bears against a shoulder surface 812 on the first part when both parts are embedded in bone. When both parts are assembled into an anchoring element 800 by being embedded in bone, the second part 820 may be adjusted to change the distally directed pressure of the first part 810 against the bone.

5 [0085] Figures 28 through 30 show another anchoring element 900 that embodies the invention. A first part 910 includes a first surface 901, a second surface 902, and a third surface 903. The third surface 903 extends from the distal end to the proximal end providing a through passage that includes an internal thread for a least a portion of the third surface. A second part 920 includes a fourth surface 904, a fifth surface 905, and a sixth surface 906. The second part 920 further includes a joining surface 922 that is generally cylindrical and concentric with the fifth surface 905. At least a portion of the joining surface may include an external thread that mates with at least a portion of the threaded third surface 903 of the first part 910. The third surface 903 is joined to the fourth surface 904 by screwing the second part 920 into the first part 910. The resulting assembly provides an anchoring element 900 that has similar features to the anchoring element 300 shown in Figure 9.

15 [0086] Figure 31 shows another anchoring element 1000 that embodies the invention. This embodiment includes a first surface 1001, a second surface 1002, a third surface 1003, a fourth surface 1004, a fifth surface 1005, and a sixth surface 1006 similarly arranged to previously described embodiments. In this embodiment the second surface 1002, fourth surface 1004, and sixth surface 1006 may be curved. In this embodiment, only the first surface 1001 may include a threaded portion. The fifth surface 1005 may be a right cylinder such that this portion of the anchoring element 1000 may fit into a pilot hole that may have been used to guide the preparation of the bone to receive the anchoring element. The second surface 1002 may include a conical portion to provide a close fit to residual bone.

25 [0087] Figure 32 shows another anchoring element 1100 that embodies the invention. This embodiment includes a first surface 1101, a second surface 1102, a third surface 1103, a fourth surface 1104, a fifth surface 1105, and a sixth surface 1106 similarly arranged to previously described embodiments. The anchoring element 1100 of this embodiment is generally similar to the anchoring element 1000 of Figure 31. The fifth surface 1105 and the second surface 1102 may include conical portions to provide a close fit to residual bone.

[0088] Figure 33 shows another anchoring element 1200 that embodies the invention. Figure 33 is a cross-section of the anchoring element 1200 embedded in the posterior portion of a mandible along section line in a bucco-lingual (cheek to tongue) direction. This embodiment includes an abutment surface 1210 that is at an angle to an axis from the proximal end to the distal end of the first surface. The abutment surface 1210 may be substantially flat in the area adjacent the proximal end of the first surface 1201. As shown in Figure 33, when an anchoring element is embedded in a healed molar extraction site, resorption of the bone may cause the site to be shallow with a surface that may be higher on one side 1220 than the other 1222, generally being lower to the buccal (cheek) side 1222. It may be seen that the angled abutment surface 1210 allows the first surface 1201 to have greater contact with the bone without leaving a portion of the anchoring element 1201 exposed above the bone.

[0089] Figure 34 shows another anchoring element 1300 that includes an abutment surface 1310 that is at an angle to an axis from the proximal end to the distal end of the first surface.

[0090] Figure 35 shows another anchoring element 1400 that includes an abutment surface 1410 that is at an angle to an axis from the proximal end to the distal end of the first surface. In this embodiment the threaded portion of the first surface may extend to the abutment surface which may increase the threaded engagement of the anchoring element 1400 to bone.

[0091] While certain exemplary embodiments have been described and shown in the accompanying drawings, it is to be understood that such embodiments are merely illustrative of and not restrictive on the broad invention, and that this invention not be limited to the specific constructions and arrangements shown and described, since various other modifications may occur to those ordinarily skilled in the art. It is to be understood that individual features shown or described for one embodiment may be combined with individual features shown or described for another embodiment. It is to be understood some features are shown or described to illustrate the use of the invention in the context of functional anchoring

elements and such features may be omitted within the scope of the invention.

CLAIMS

What is claimed is:

CLAIMS

What is claimed is:

1. An anchoring element for use in bone, the anchoring element comprising:
a first surface having a distal end and a proximal end, at least a portion of
the first surface including a first external thread having a pitch;
an abutment surface disposed toward the proximal end of the first surface;
an annular second surface disposed toward the distal end of the first
surface and joined to the first surface along an outer circumference
of the second surface;
a third surface concentric with the first surface and joined to the second
surface along an inner circumference of the second surface, at least
a portion of the third surface including an internal thread having the
pitch of the first external thread; and
a fourth surface disposed between the distal end and the proximal end of
the first surface and joined to the third surface along an outer
circumference of the fourth surface.
2. The anchoring element of claim 1 wherein the first surface includes a
frustrated first conical portion adjacent the distal end such that a smaller
circumference of the first conical portion is adjacent the distal end.
3. The anchoring element of claim 1 wherein the third surface includes a
frustrated second conical portion adjacent the distal end such that a larger
circumference of the second conical portion is adjacent the distal end.
4. The anchoring element of claim 1 wherein the fourth surface is annular,
the anchoring element further comprising:
a fifth surface concentric with the first surface and joined to the fourth
surface along an inner circumference of the fourth surface, at least
a portion of the fifth surface including a second external thread
having the pitch of the first external thread; and

a sixth surface disposed toward the distal end of the first surface and joined to the fifth surface along an outer circumference of the sixth surface.

5. The anchoring element of claim 4 wherein the fifth surface includes a frustrated third conical portion adjacent the distal end such that a smaller circumference of the third conical portion is adjacent the distal end.
6. The anchoring element of claim 4 wherein the first surface, the second surface, the third surface, and the fourth surface are on a first part, the fifth surface and the sixth surface are on a second part, and the fifth surface is placed adjacent to the fourth surface by passing the second part through the first part.
7. The anchoring element of claim 4 wherein the first surface, the second surface, and the third surface are on a first part, the fourth surface, the fifth surface, and the sixth surface are on a second part, and the fourth surface is placed adjacent to the third surface by passing the second part through the first part.
8. The anchoring element of claim 1 wherein the abutment surface is at an angle to an axis from the proximal end to the distal end of the first surface.
9. An anchoring element for use in bone, the anchoring element comprising:
a first surface having a distal end and a proximal end, at least a portion of the first surface including a first external thread having a pitch;
an abutment surface disposed toward the proximal end of the first surface;
an annular second surface disposed toward the distal end of the first surface and joined to the first surface along an outer circumference of the second surface;
a third surface concentric with the first surface and joined to the second surface along an inner circumference of the second surface;

an annular fourth surface disposed between the distal end and the proximal end of the first surface and joined to the third surface along an outer circumference of the fourth surface;
a fifth surface concentric with the first surface and joined to the fourth surface along an inner circumference of the fourth surface; and
a sixth surface disposed toward the distal end of the first surface and joined to the fifth surface along an outer circumference of the sixth surface.

10. An anchoring element for use in bone, the anchoring element comprising:
a first surface having a distal end and a proximal end, at least a portion of the first surface including a first external thread having a pitch; and
an abutment surface disposed toward the proximal end of the first surface at an angle to an axis from the proximal end to the distal end of the first surface.

ABSTRACT

An anchoring element for use in bone has a proximal end and a distal end. The distal end may be embedded in bone with the proximal end exposed. An abutment surface is disposed toward the proximal end. The anchoring
5 element includes four surfaces that define the distal end. A generally cylindrical first surface defines a exterior of the anchoring element. At least a portion of the first surface includes a first external thread having a pitch. An annular second surface is disposed toward the distal end and joined to the first concentric with the first surface is joined to the second surface along an inner
10 surface along an outer circumference of the second surface. A third surface circumference of the second surface. At least a portion of the third surface includes an internal thread having the pitch of the first external thread. A fourth surface disposed between the distal end and the proximal end of the first surface is joined to the third surface along an outer circumference of the fourth
15 surface.

In another embodiment, an anchoring element includes six surfaces that define the distal end. At least a portion of a first surface includes a first external thread. An annular second surface is disposed toward the distal end and joined to the first surface along an outer circumference of the second surface.
20 A third surface concentric with the first surface is joined to the second surface along an inner circumference of the second surface. An annular fourth surface is disposed between the distal end and the proximal end and joined to the third surface along an outer circumference of the fourth surface. A fifth surface concentric with the first surface is joined to the fourth surface along an inner
25 circumference of the fourth surface. A sixth surface is disposed toward the distal end and joined to the fifth surface along an outer circumference of the sixth surface.

In another embodiment, an anchoring element for use in bone has a proximal end and a distal end. The distal end may be embedded in bone with
30 the proximal end exposed. The anchoring element includes a generally cylindrical first surface, at least a portion of the first surface including an external thread. An abutment surface is disposed at the proximal end of the anchoring element. The abutment surface is at an angle to an axis from the proximal end to the distal end of the anchoring element.

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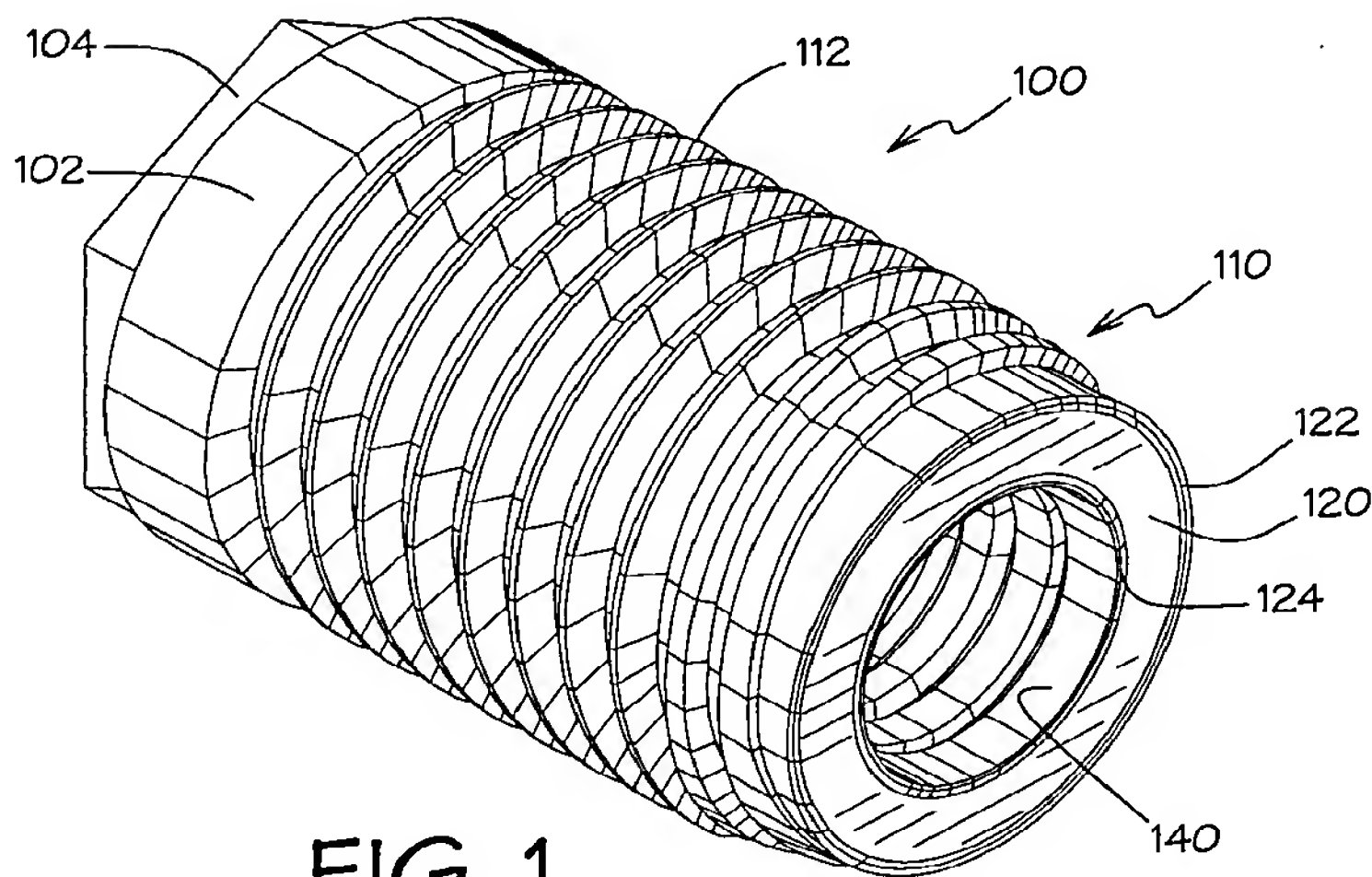


FIG. 1

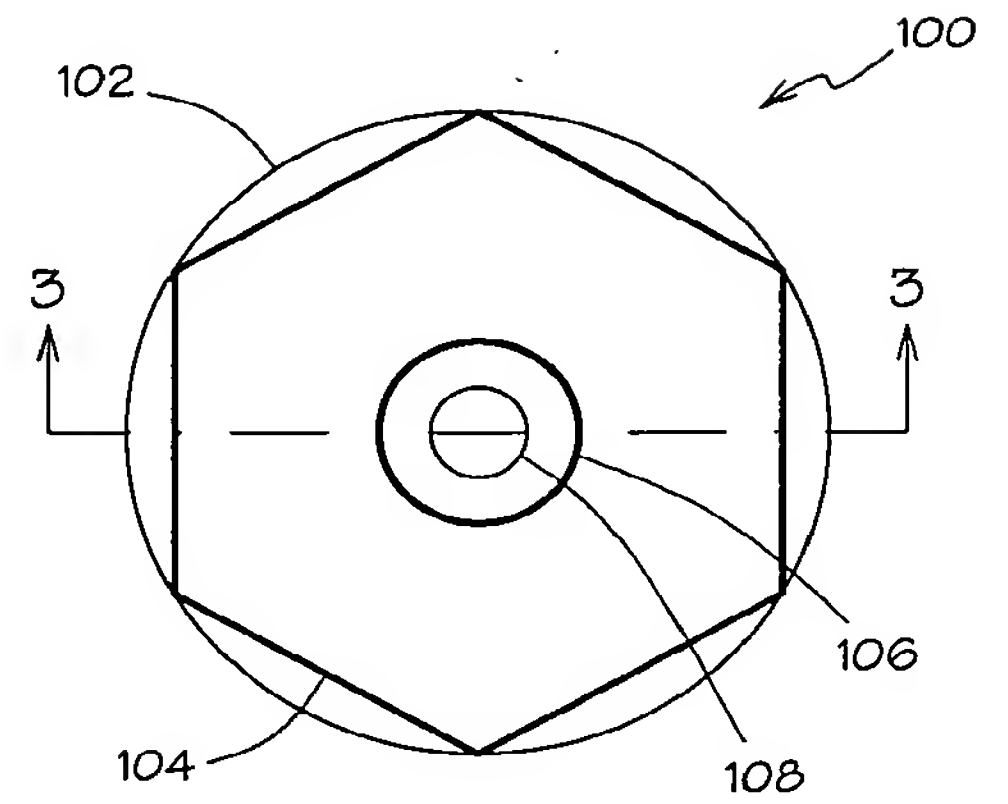


FIG. 2

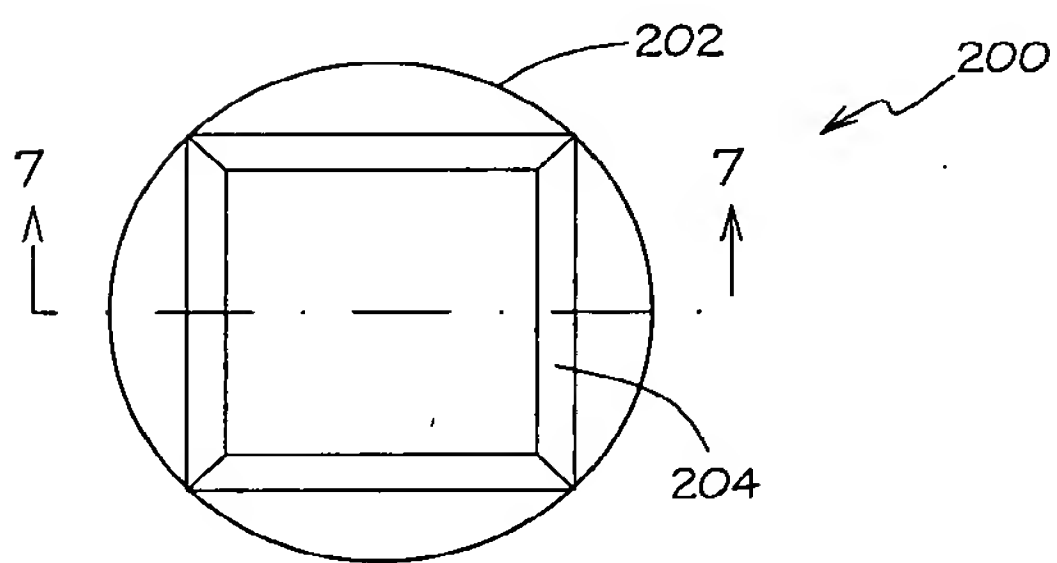


FIG. 6

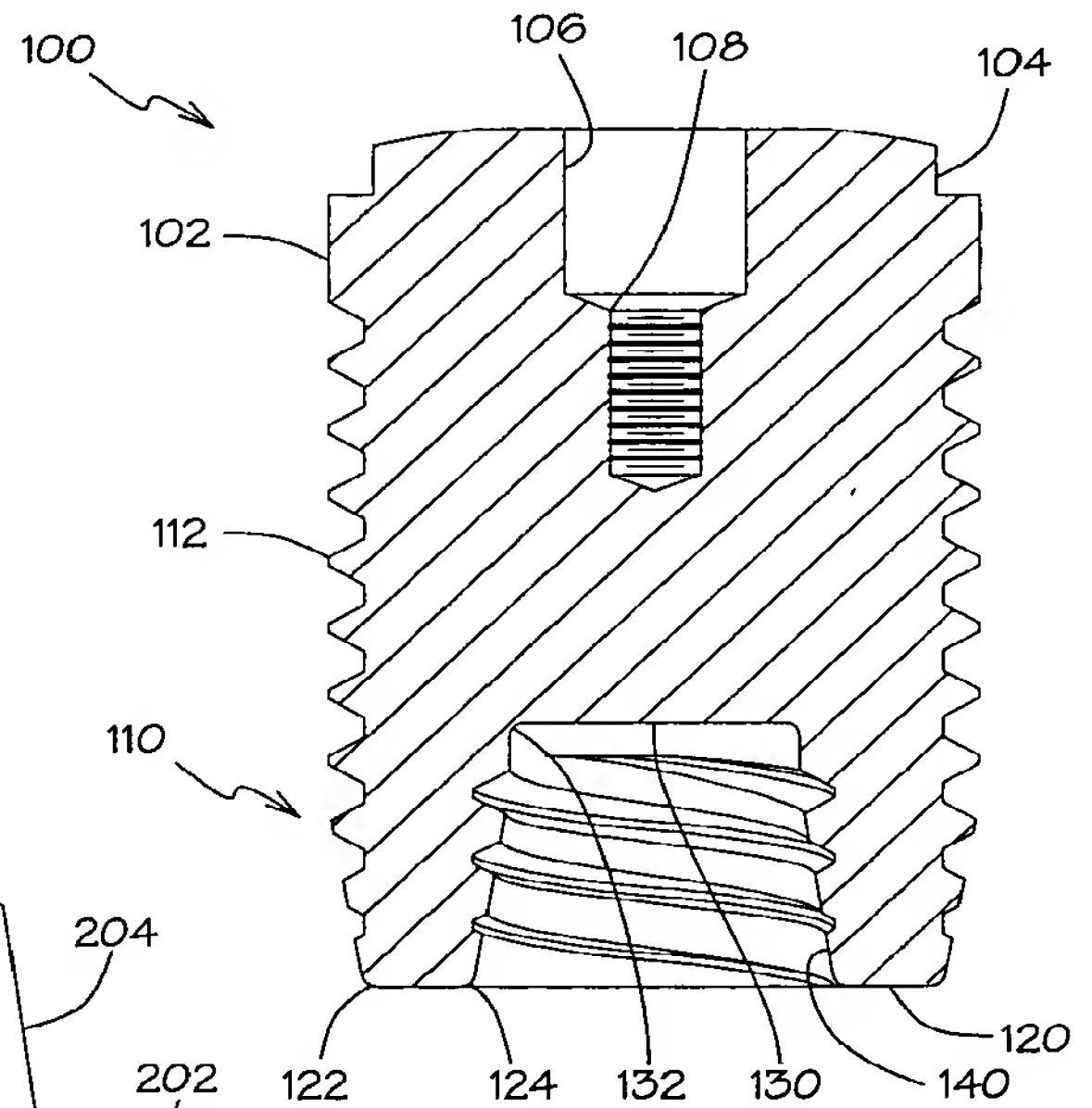


FIG. 3

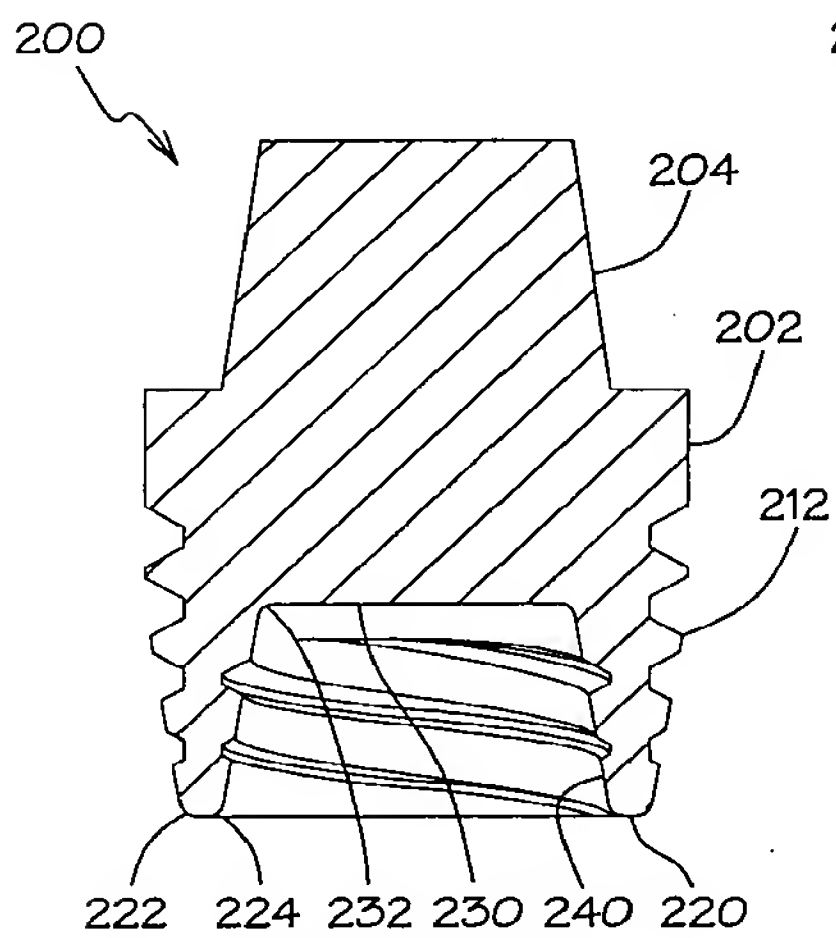


FIG. 7

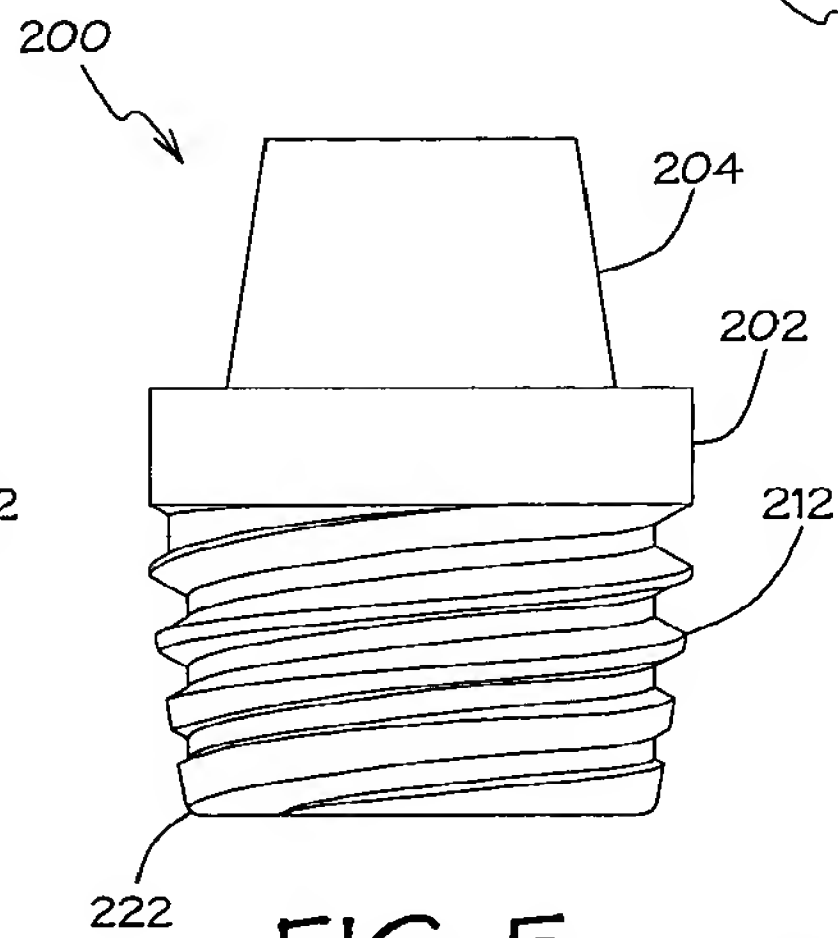


FIG. 5

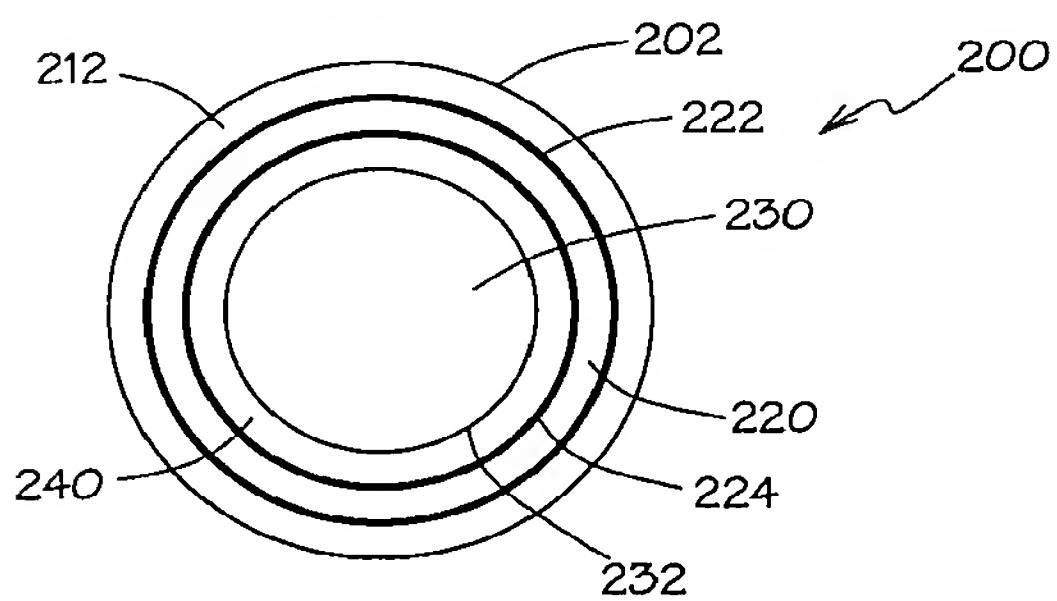


FIG. 8

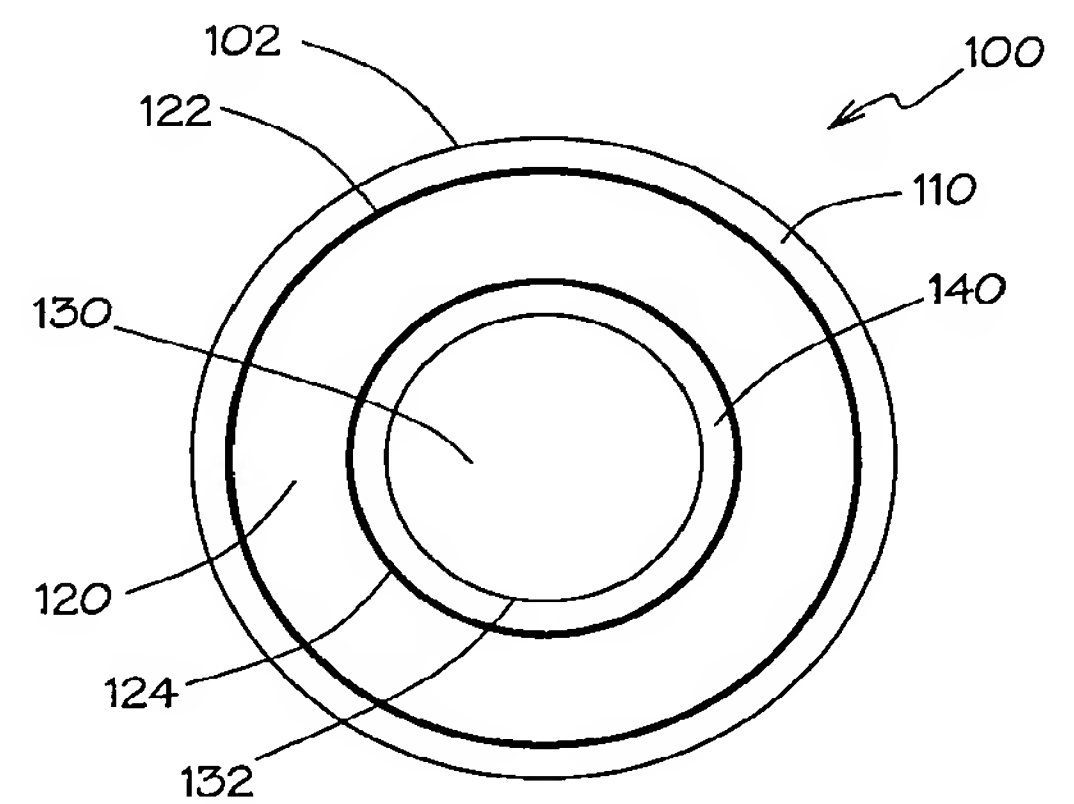
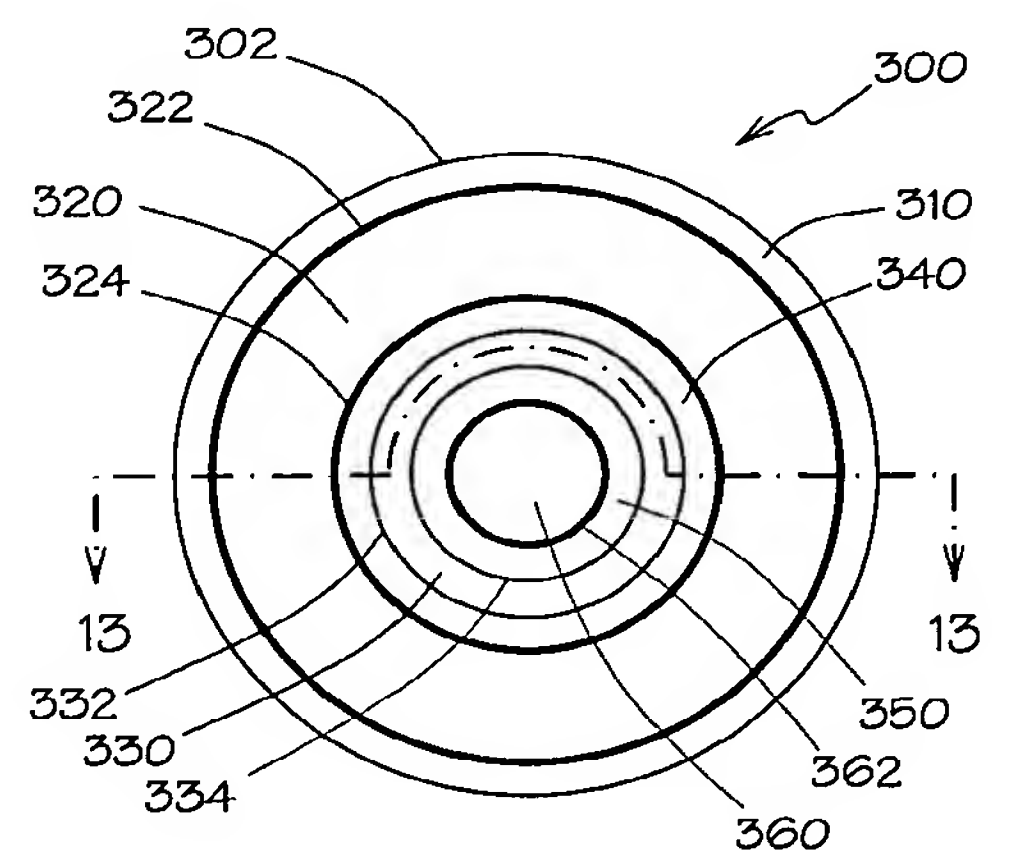
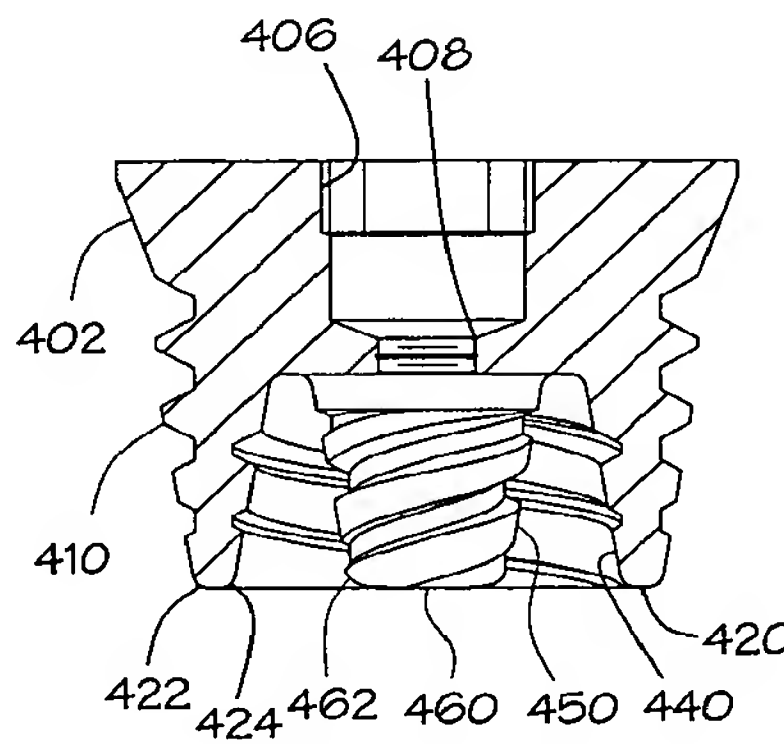
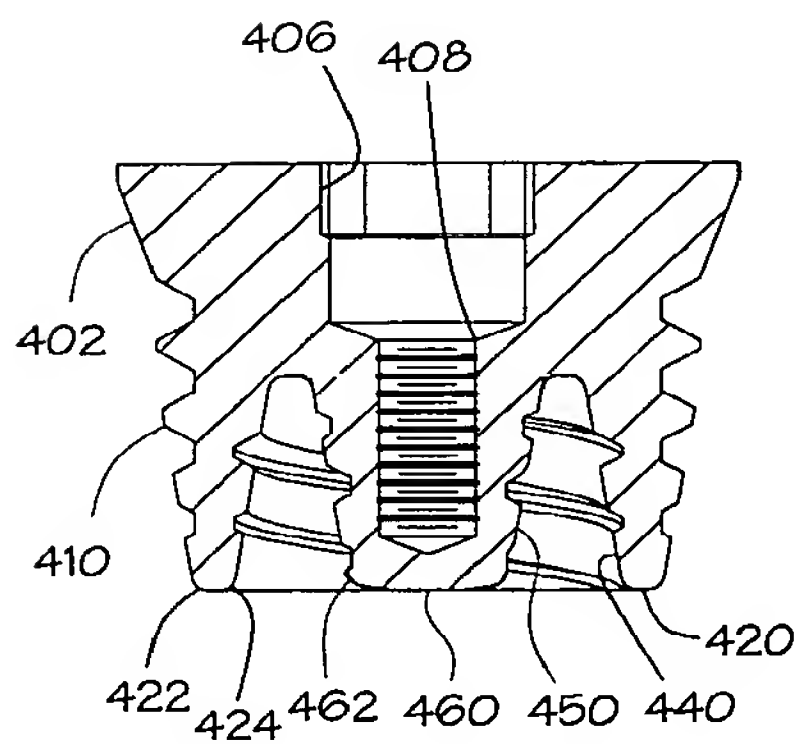
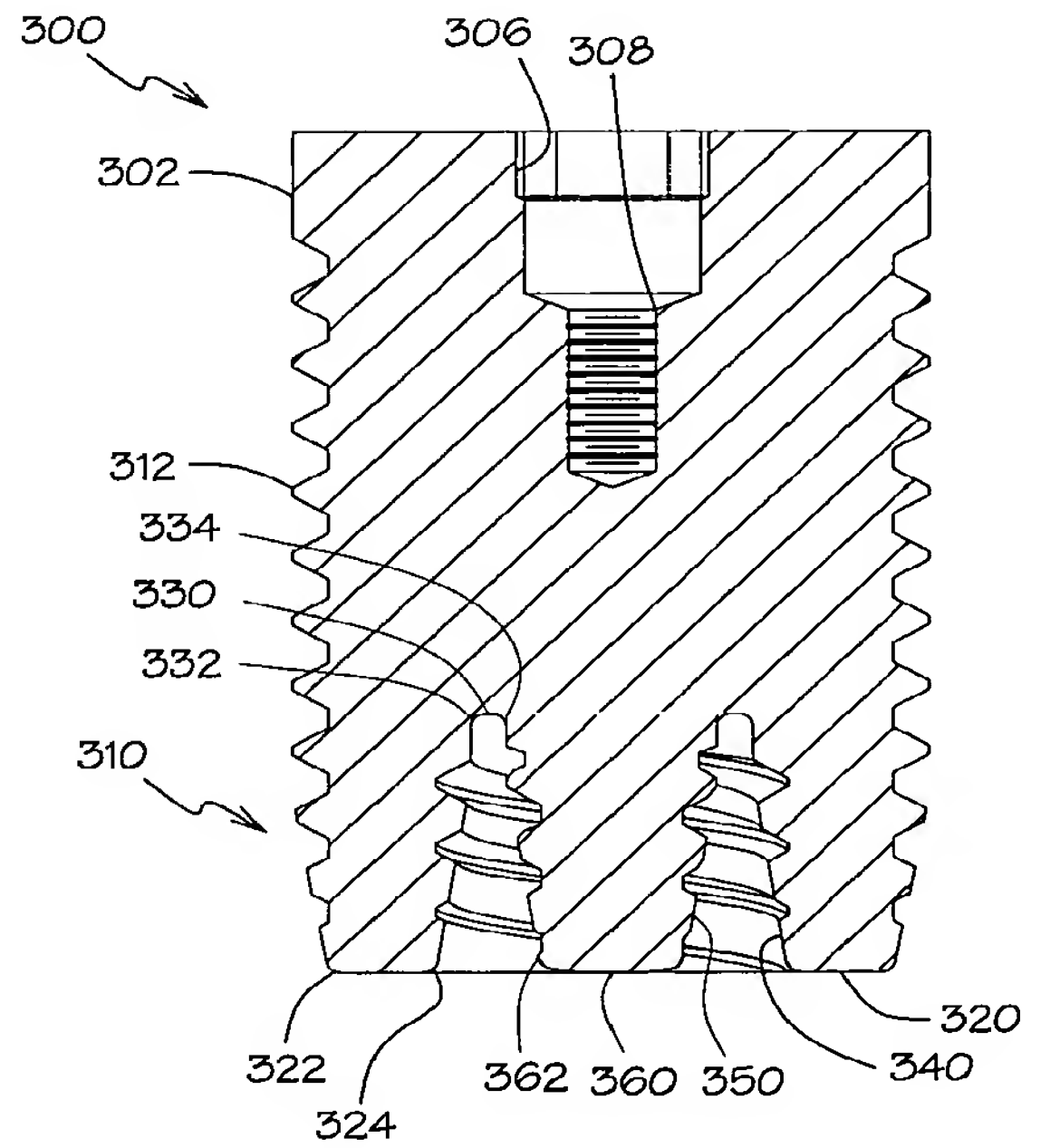
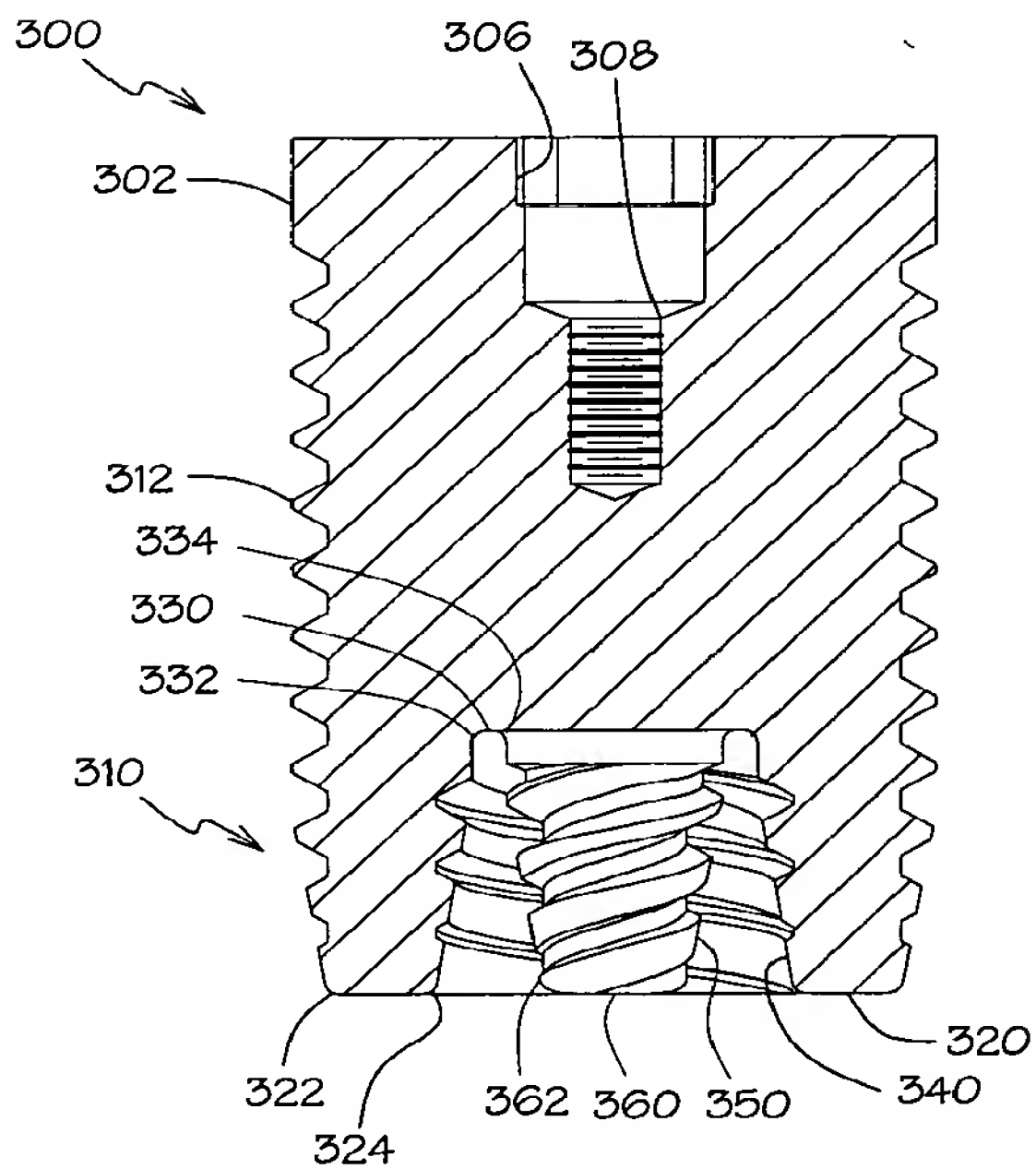
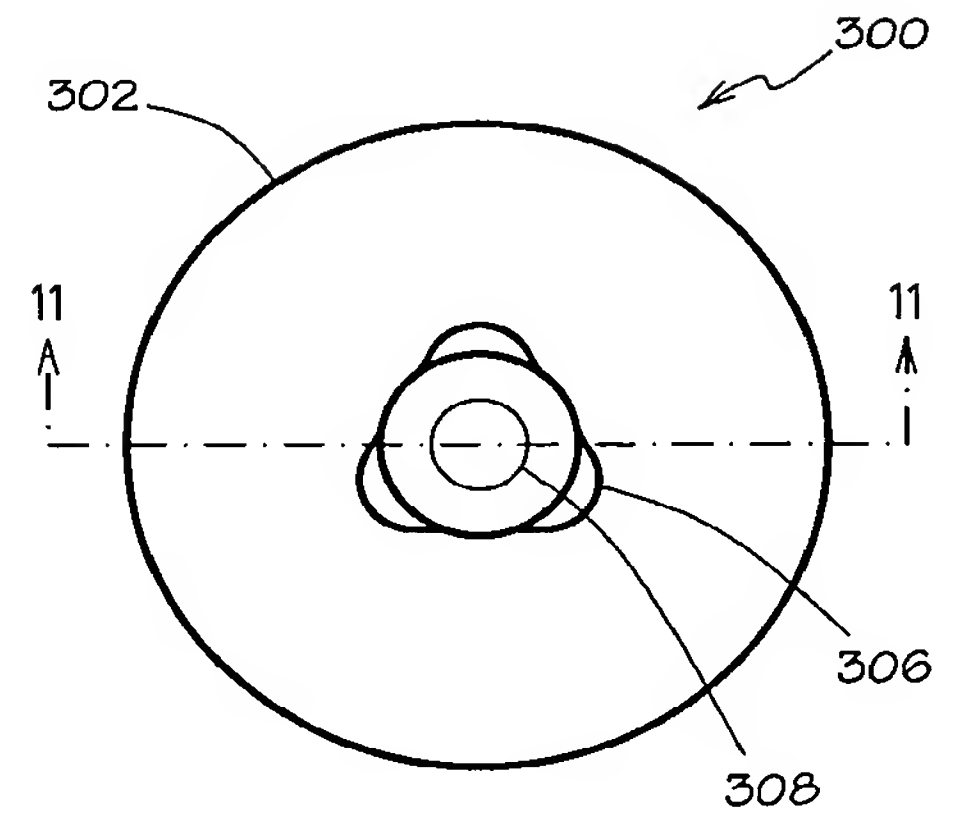
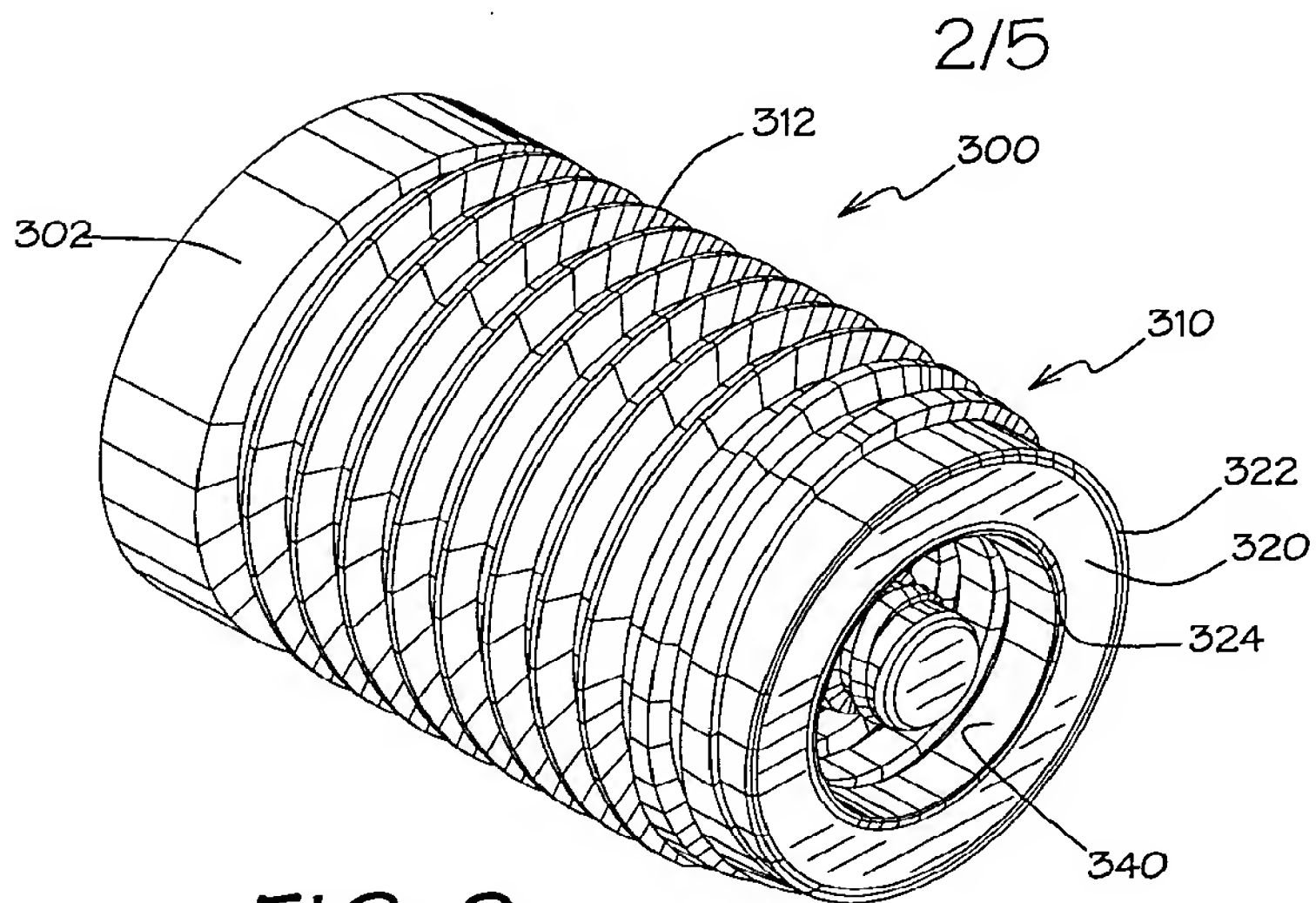


FIG. 4



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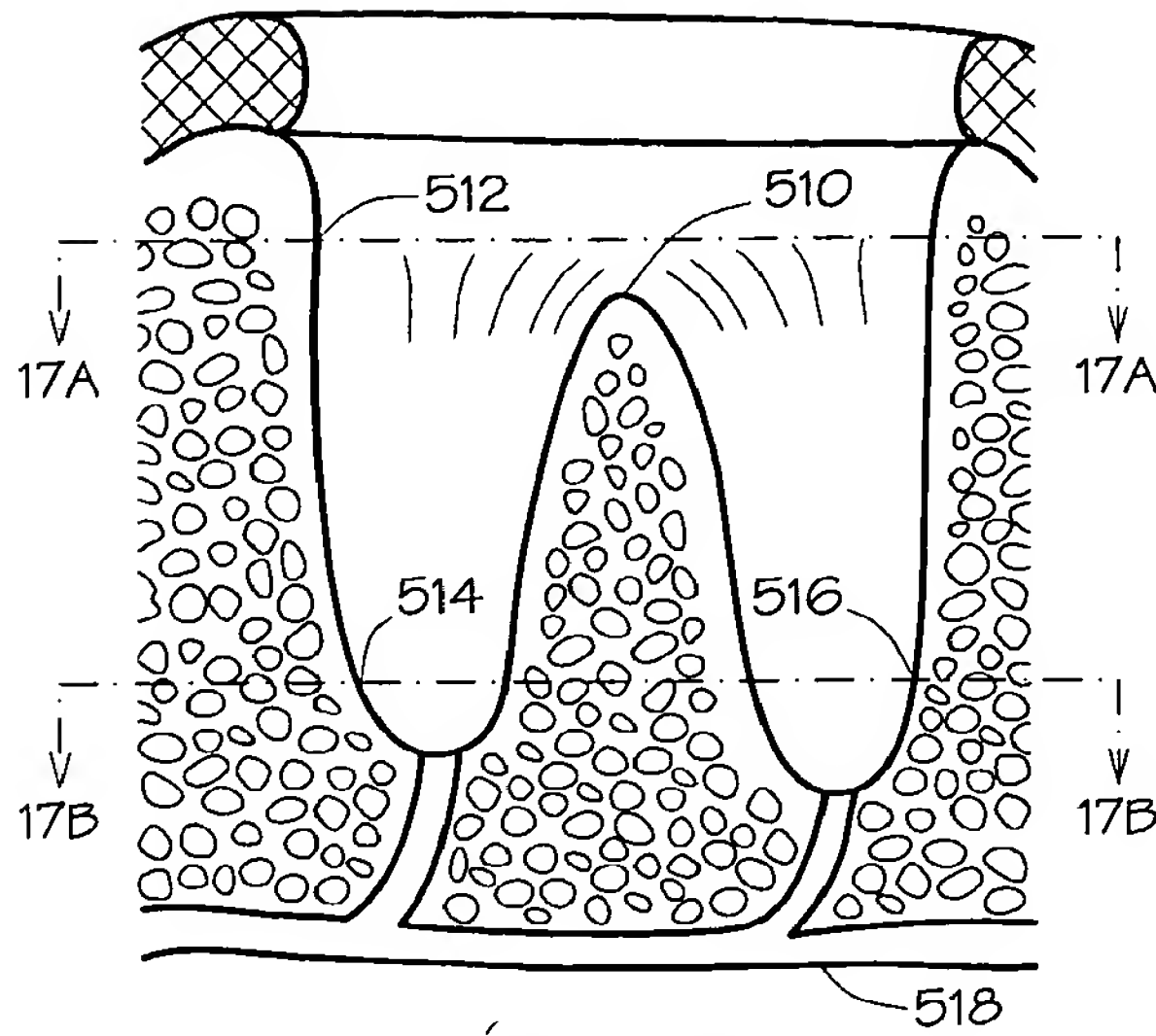


FIG. 16

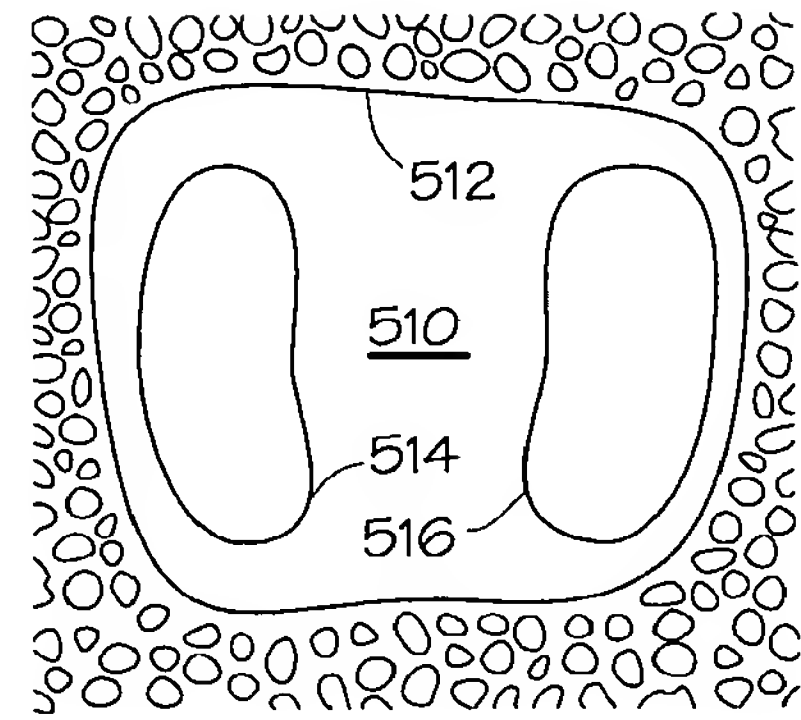


FIG. 17

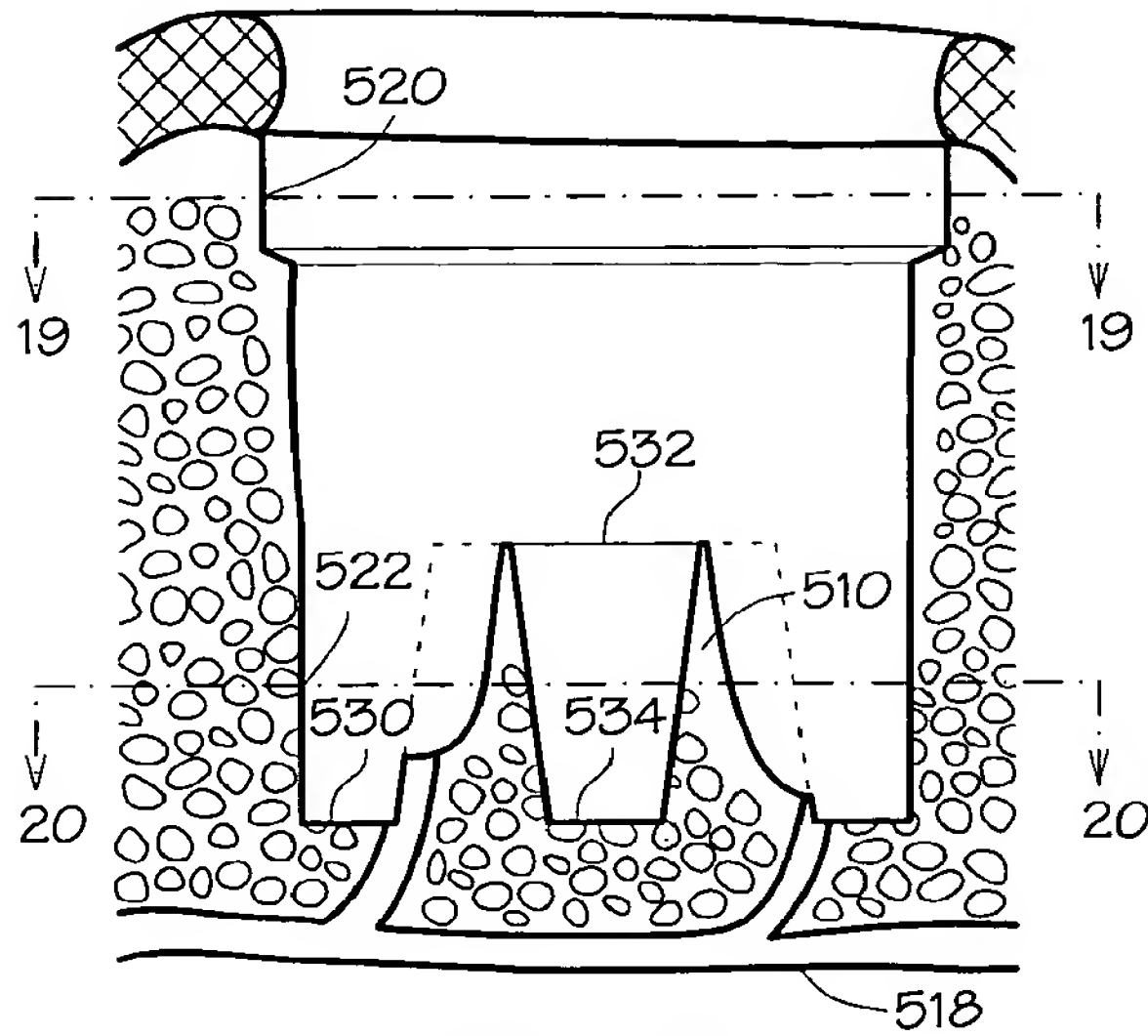


FIG. 18

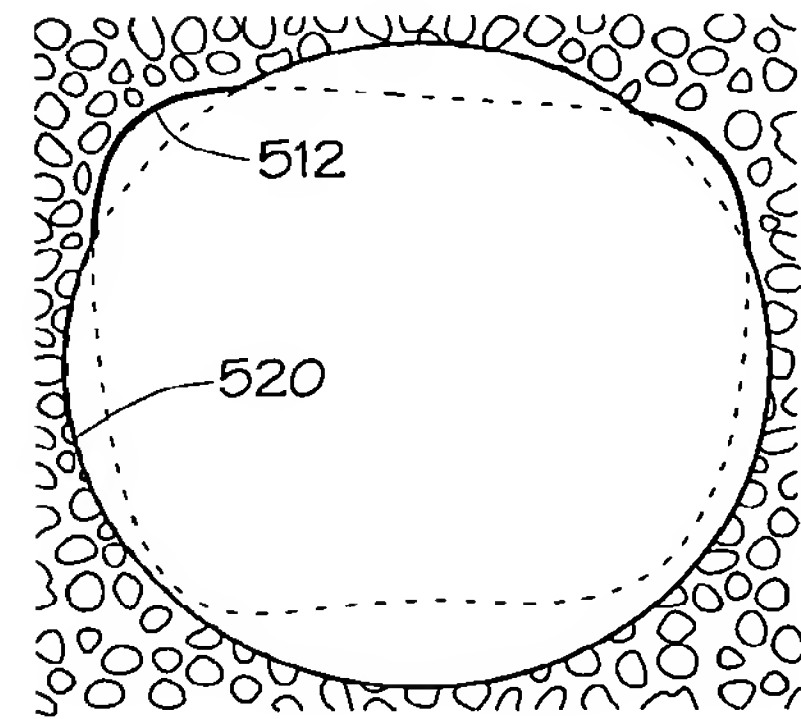


FIG. 19

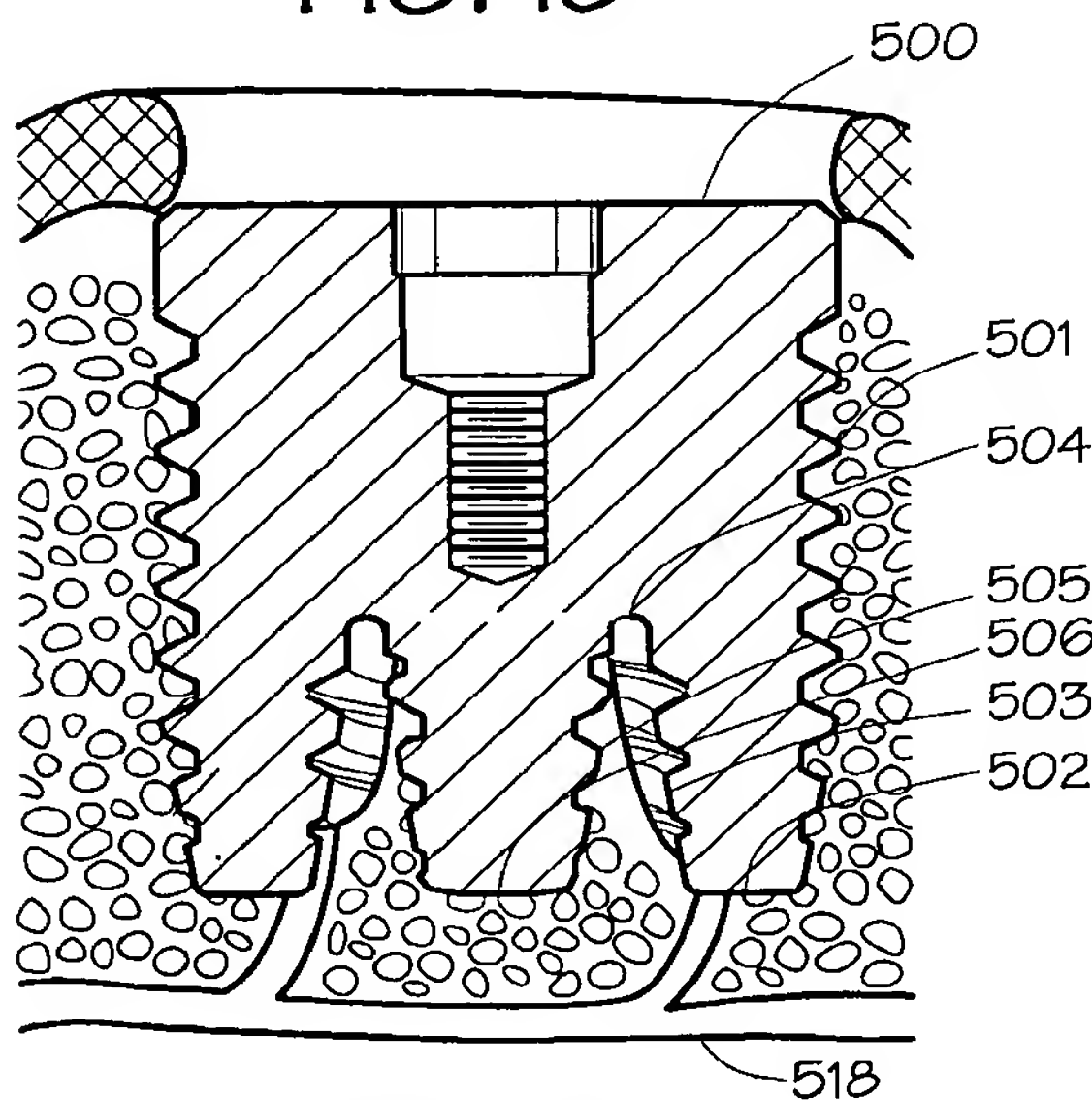


FIG. 21

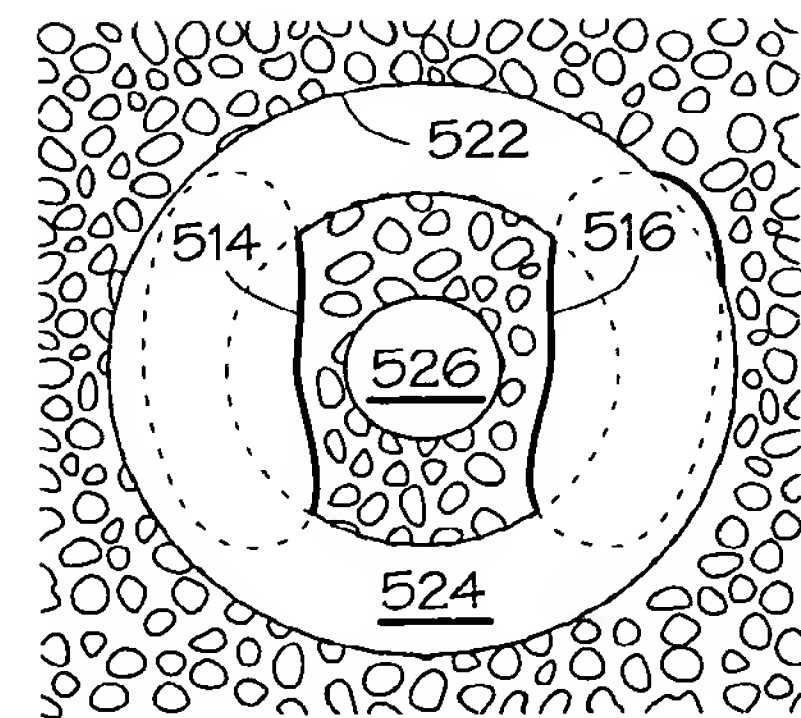


FIG. 20

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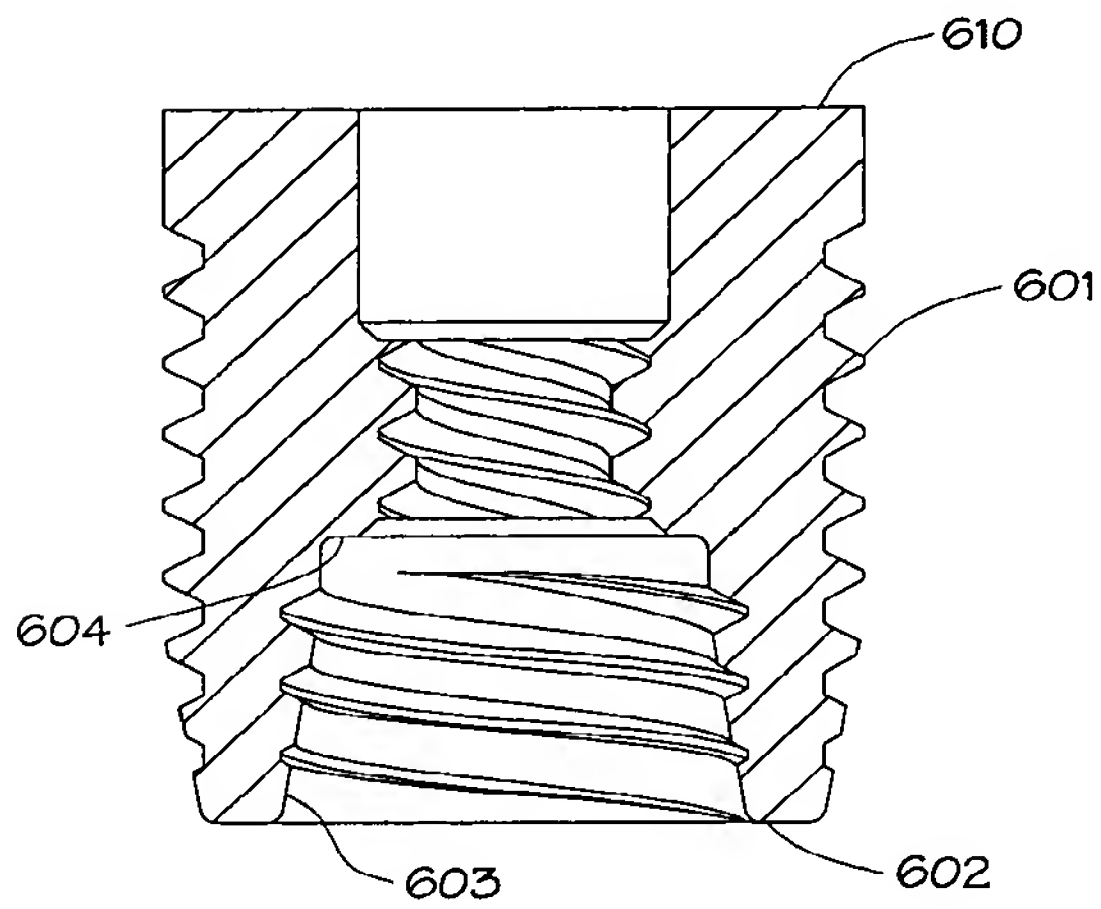


FIG. 22

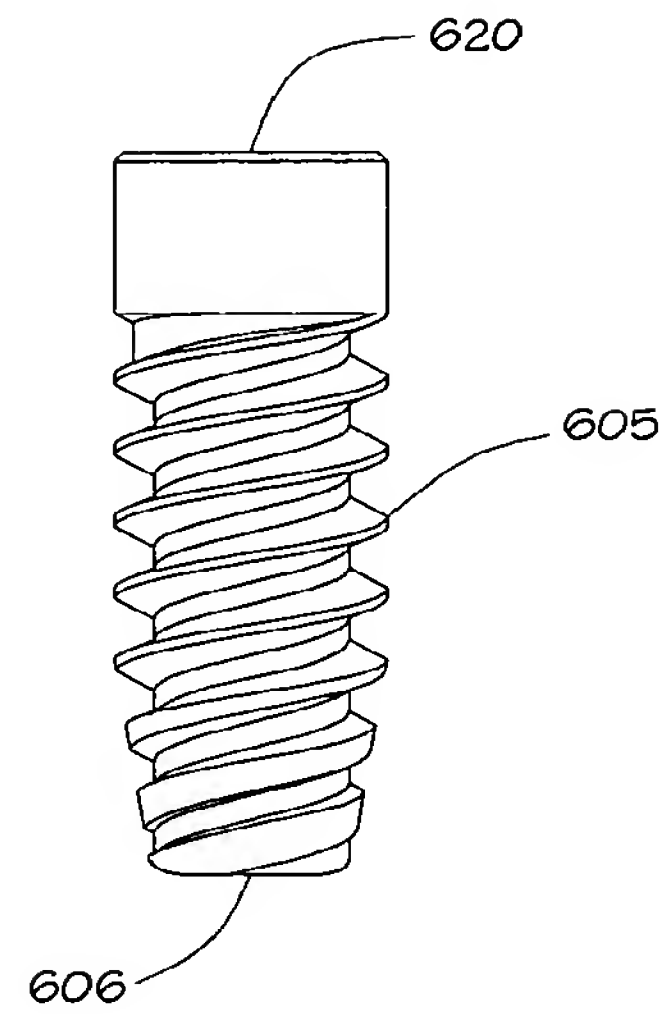


FIG. 23

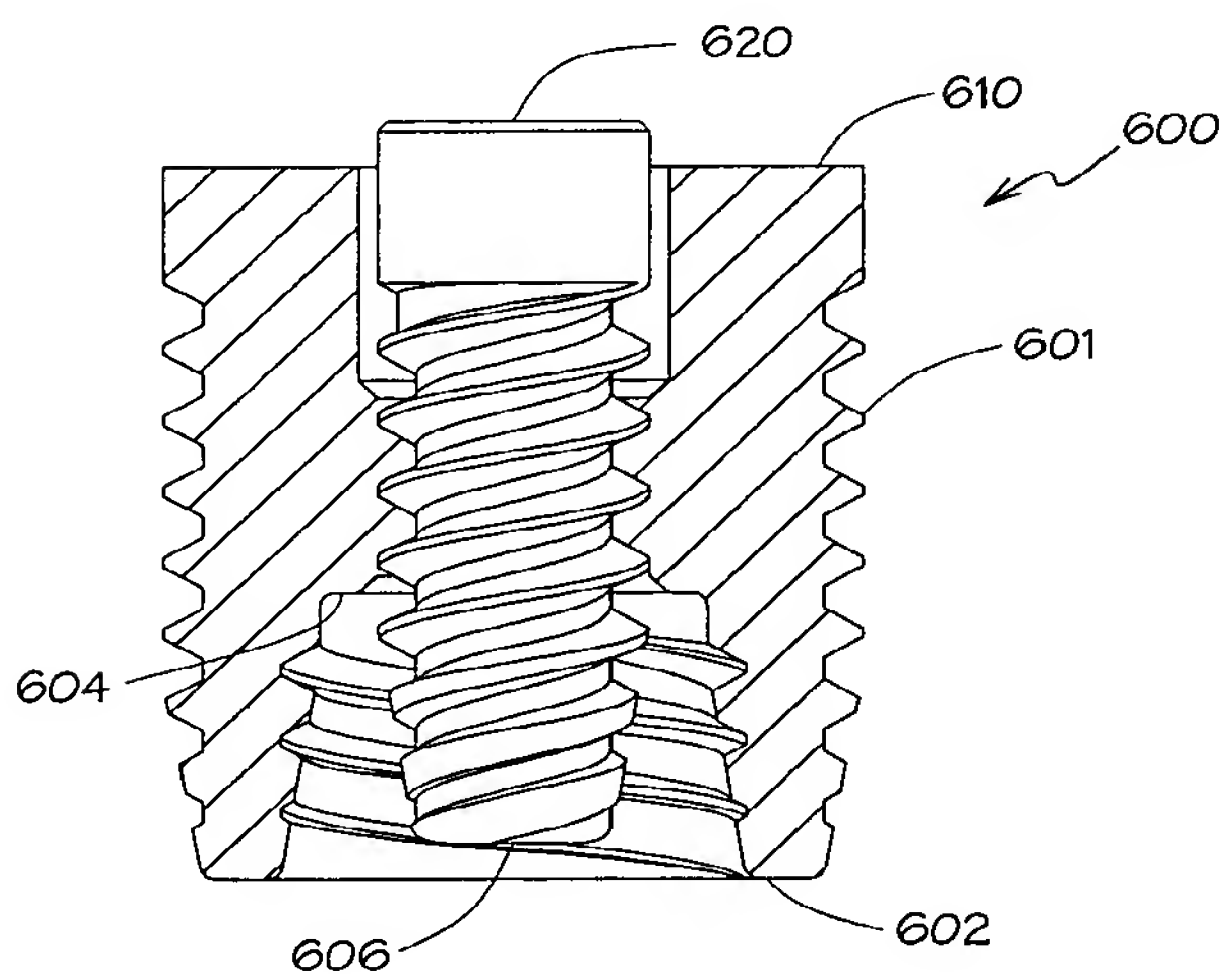


FIG. 24

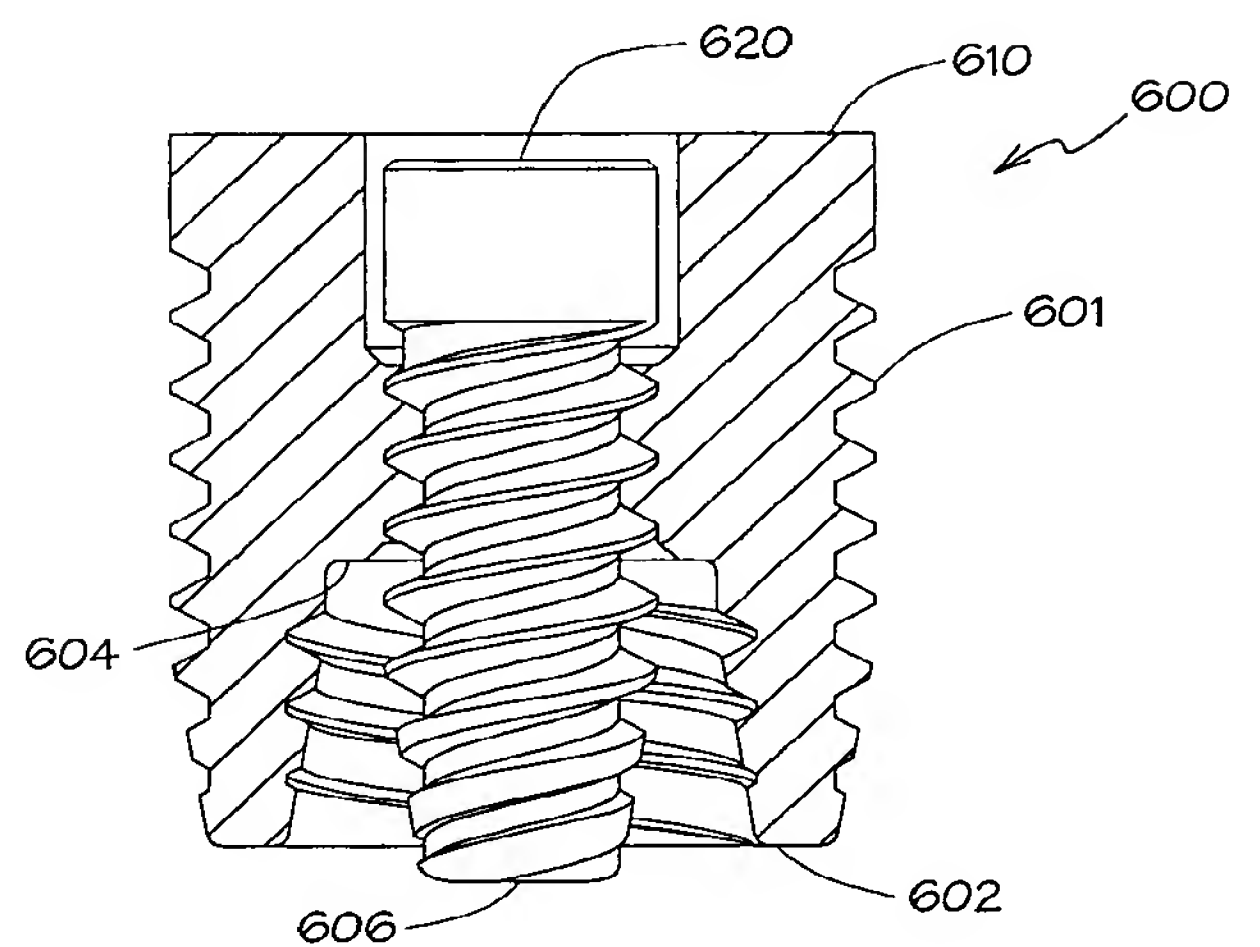


FIG. 25

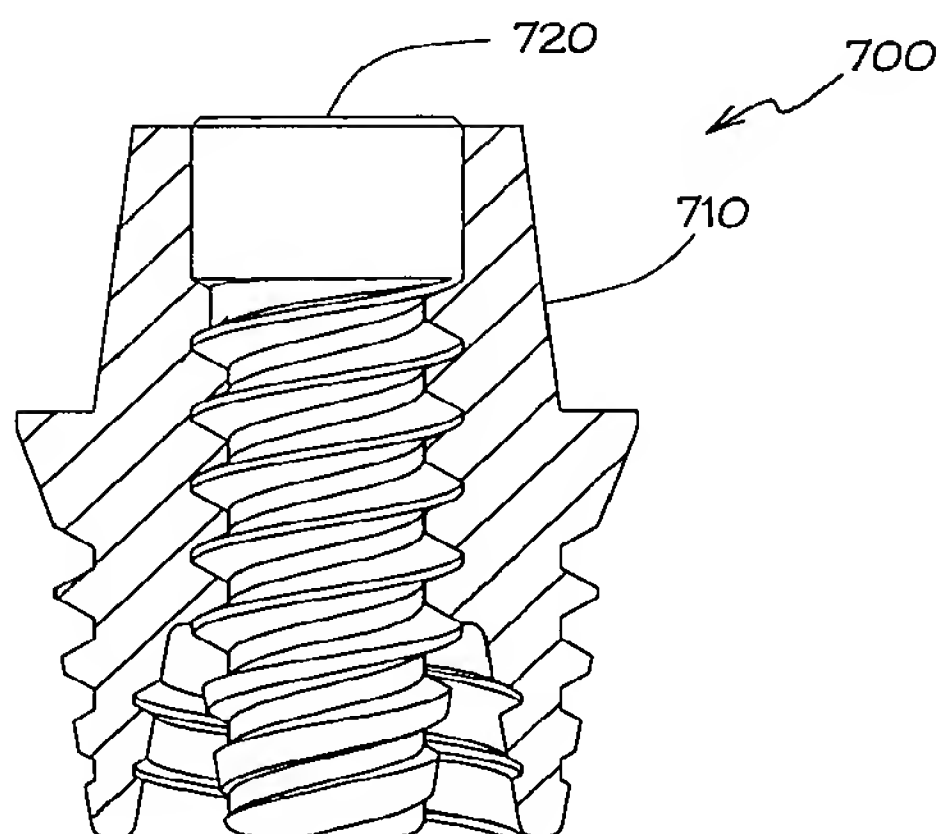


FIG. 26

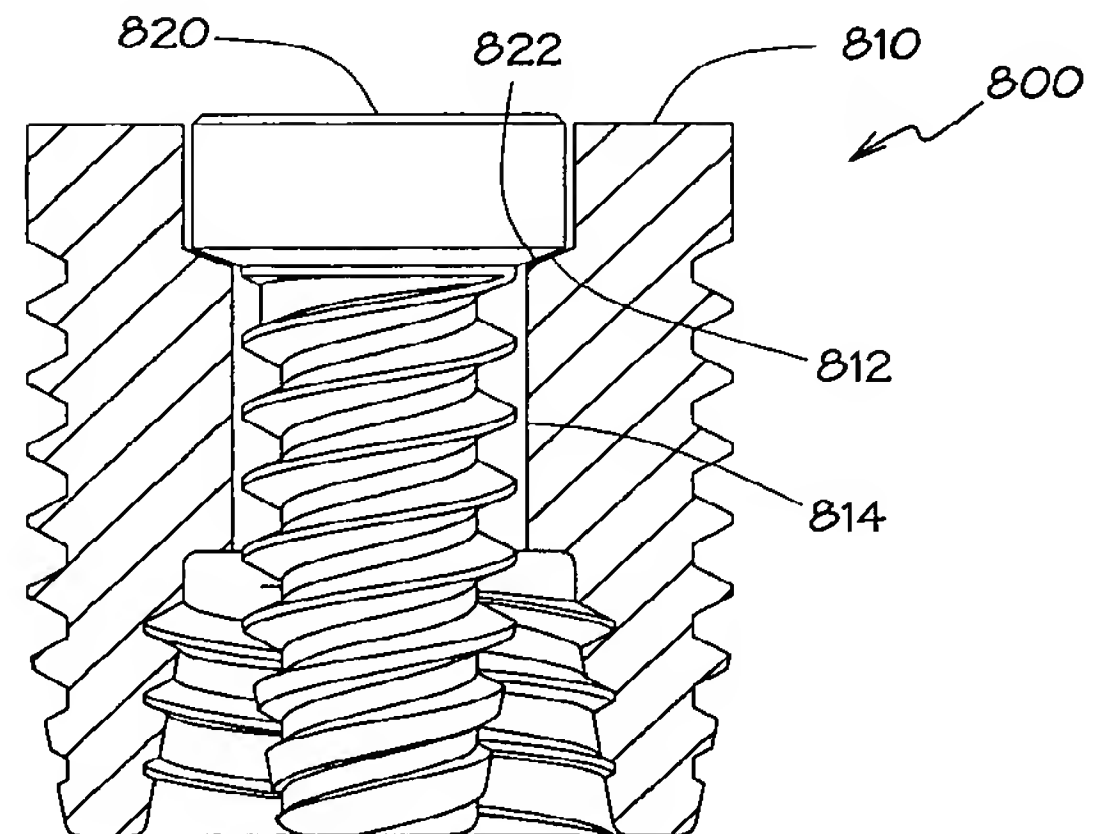


FIG. 27

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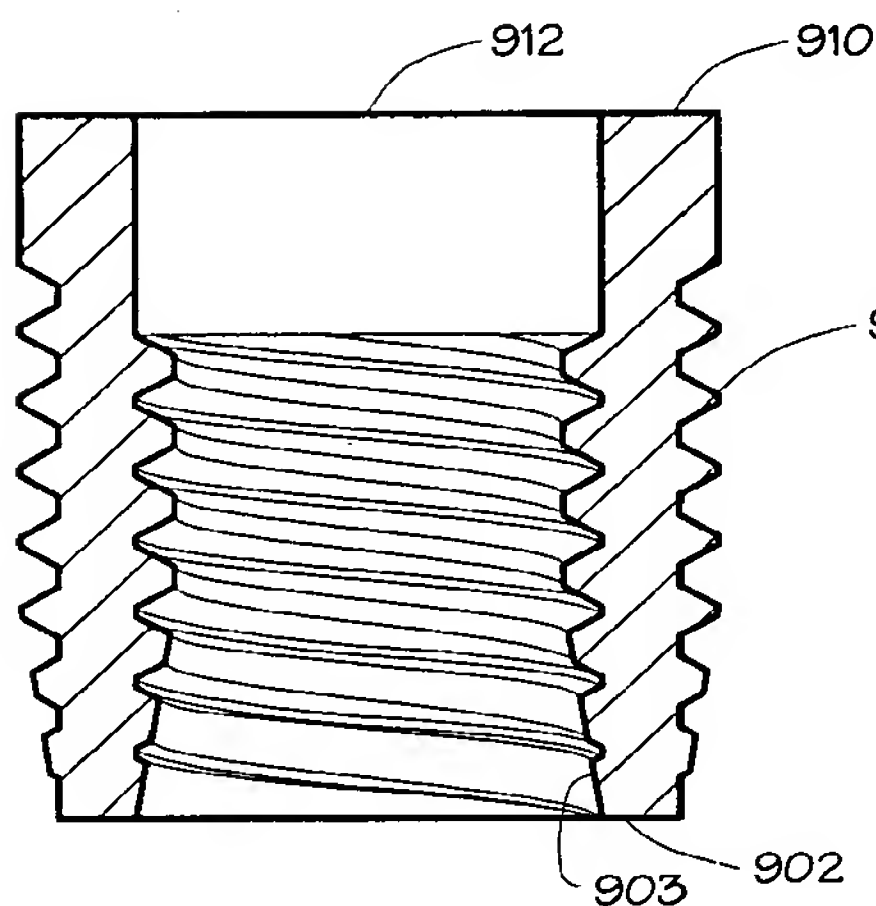


FIG. 28

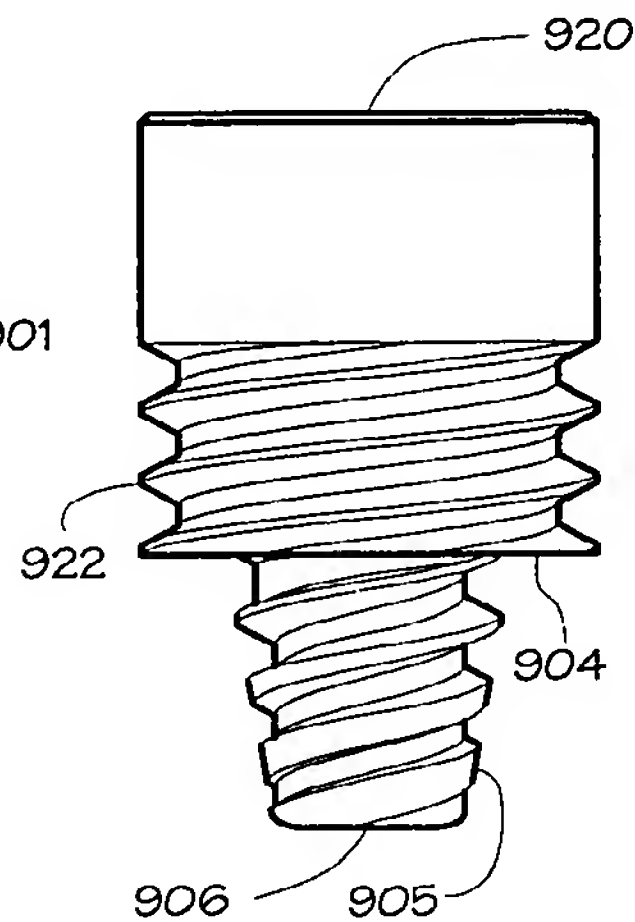


FIG. 29

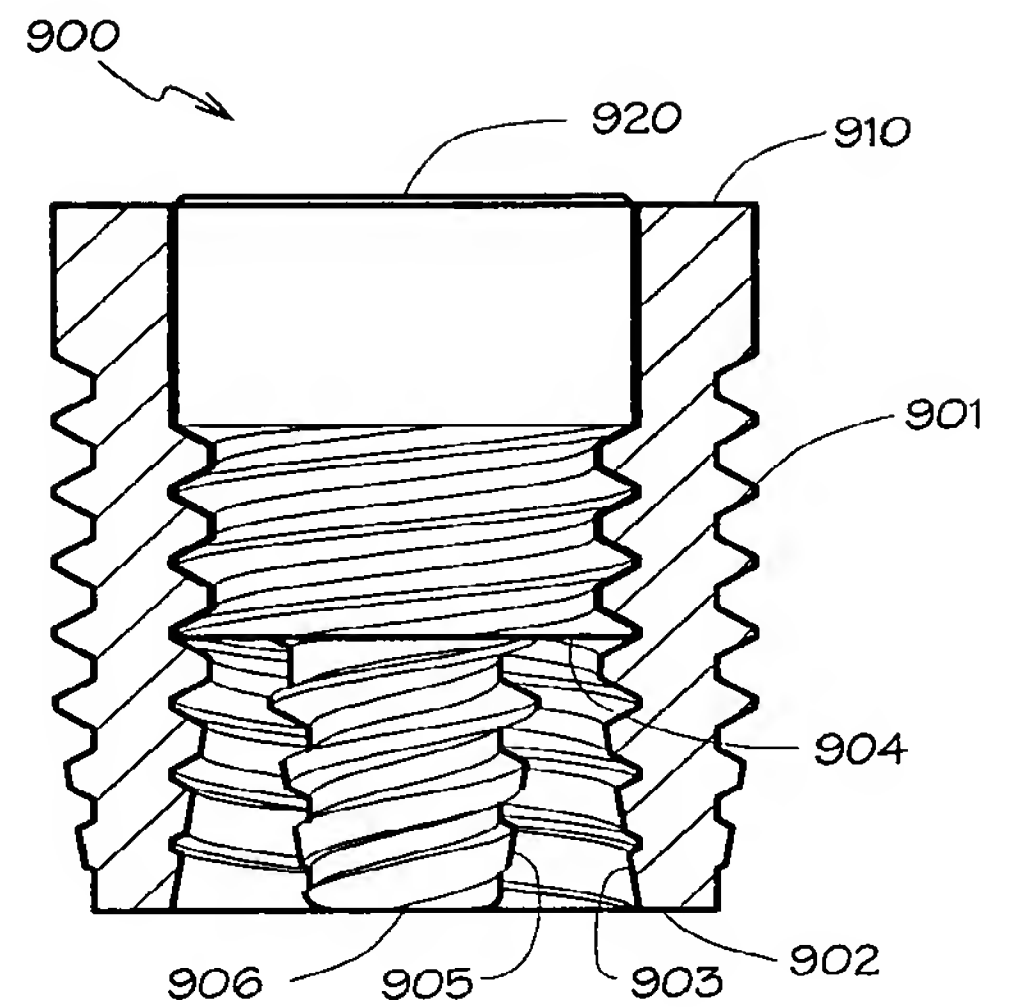


FIG. 30

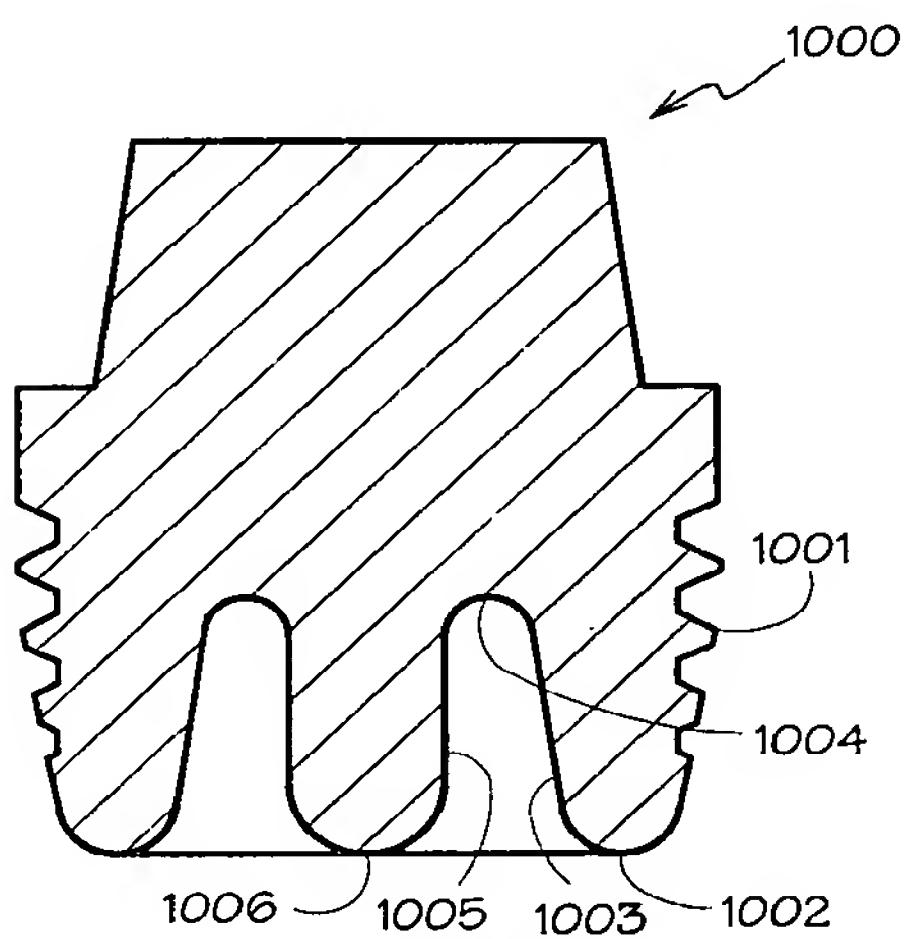


FIG. 31

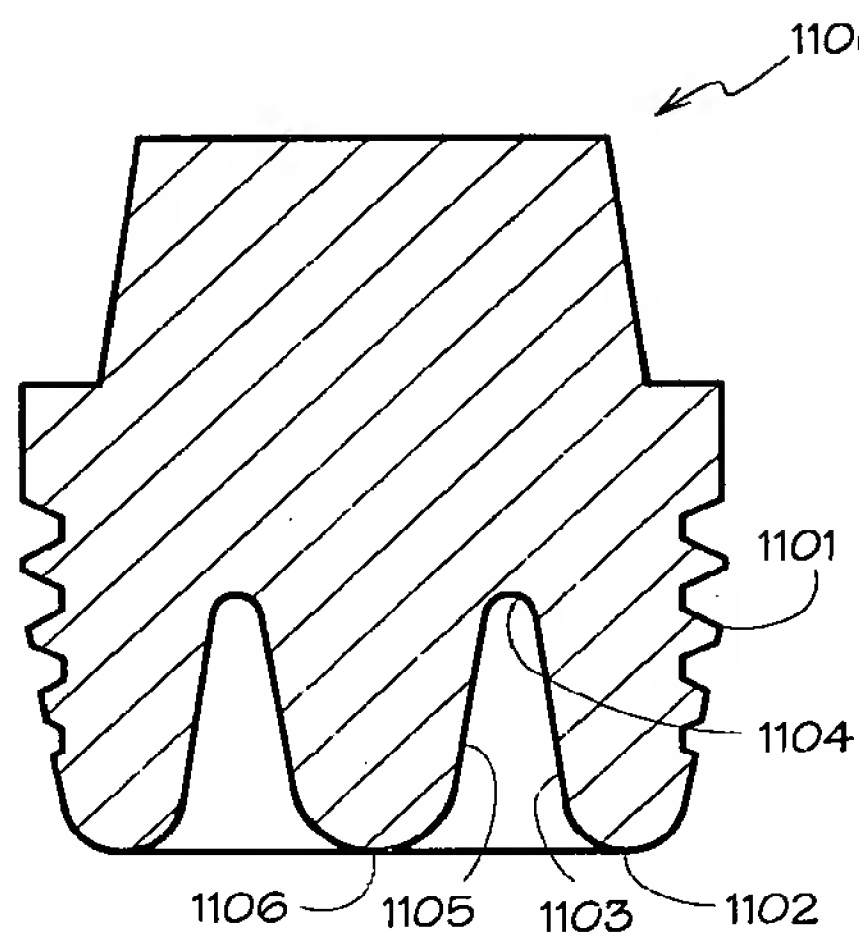


FIG. 32

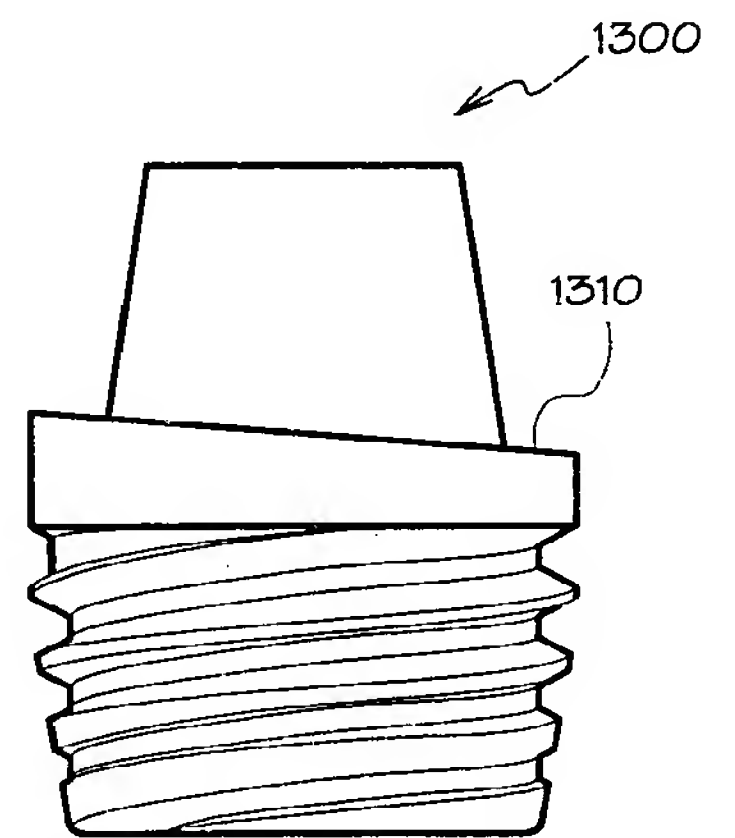


FIG. 34

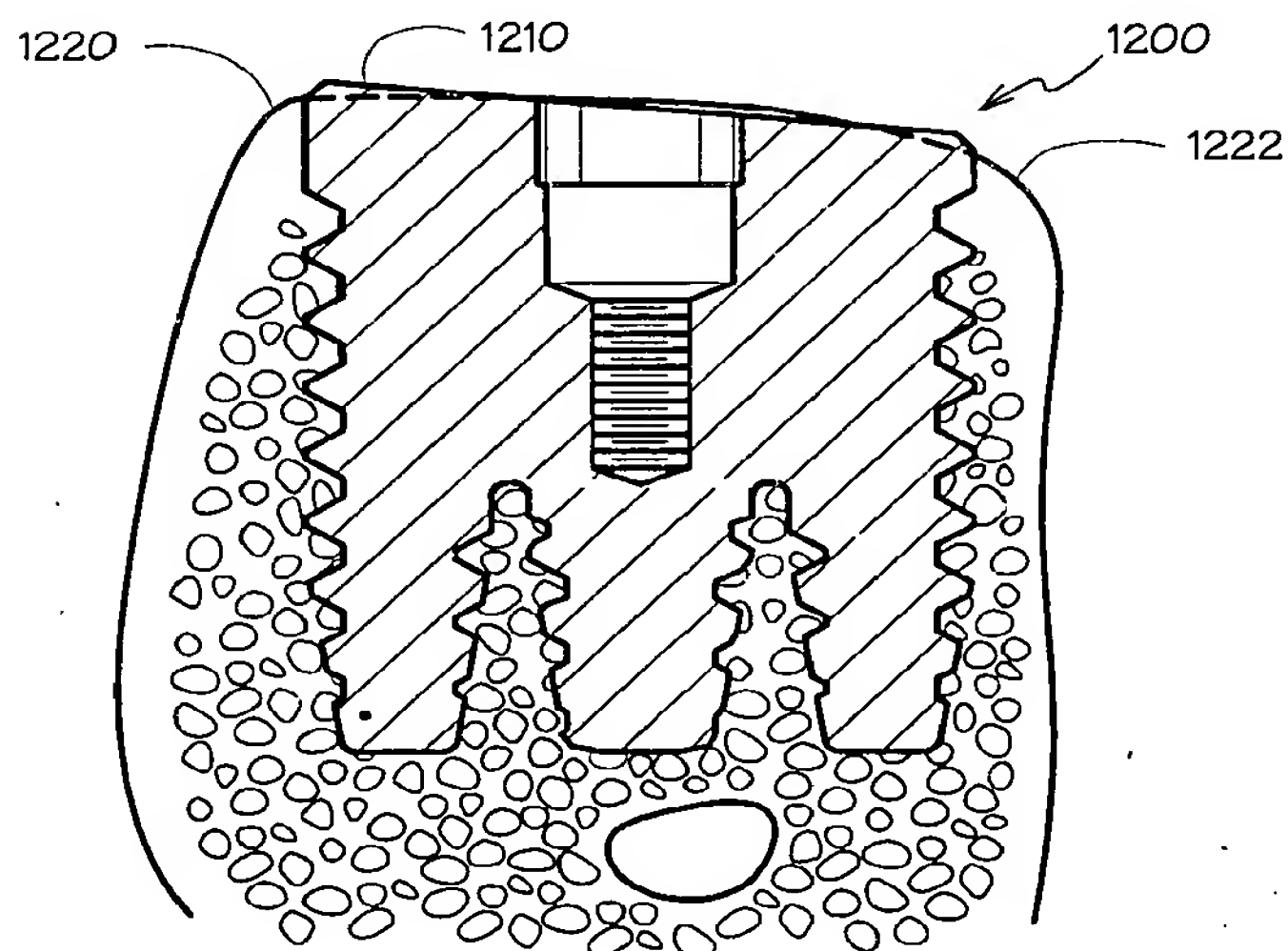


FIG. 33

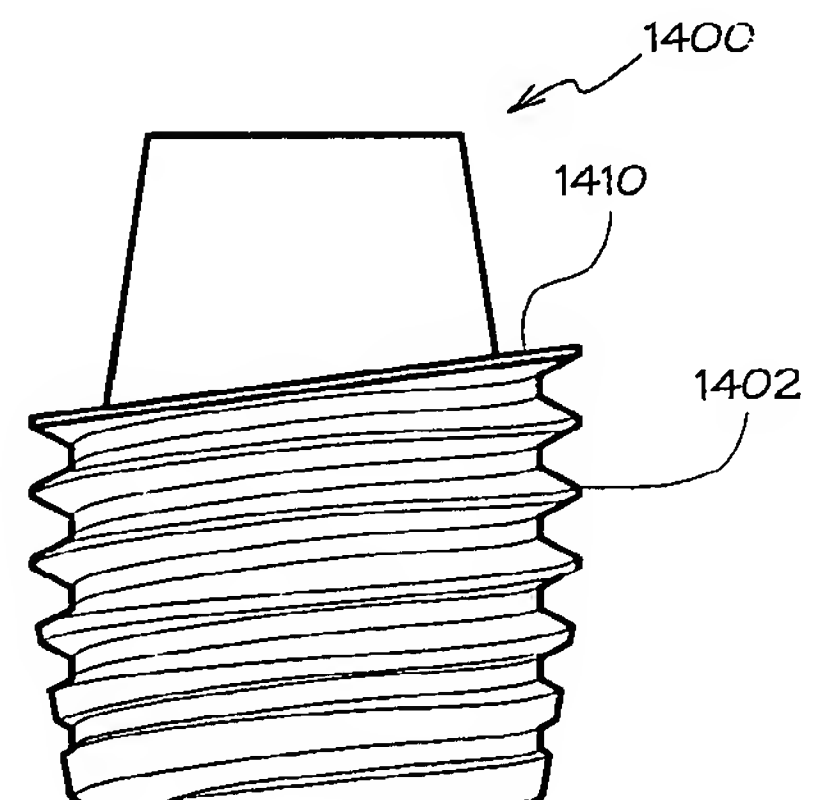


FIG. 35